

Heart rate regulation: Modeling and parameter estimation

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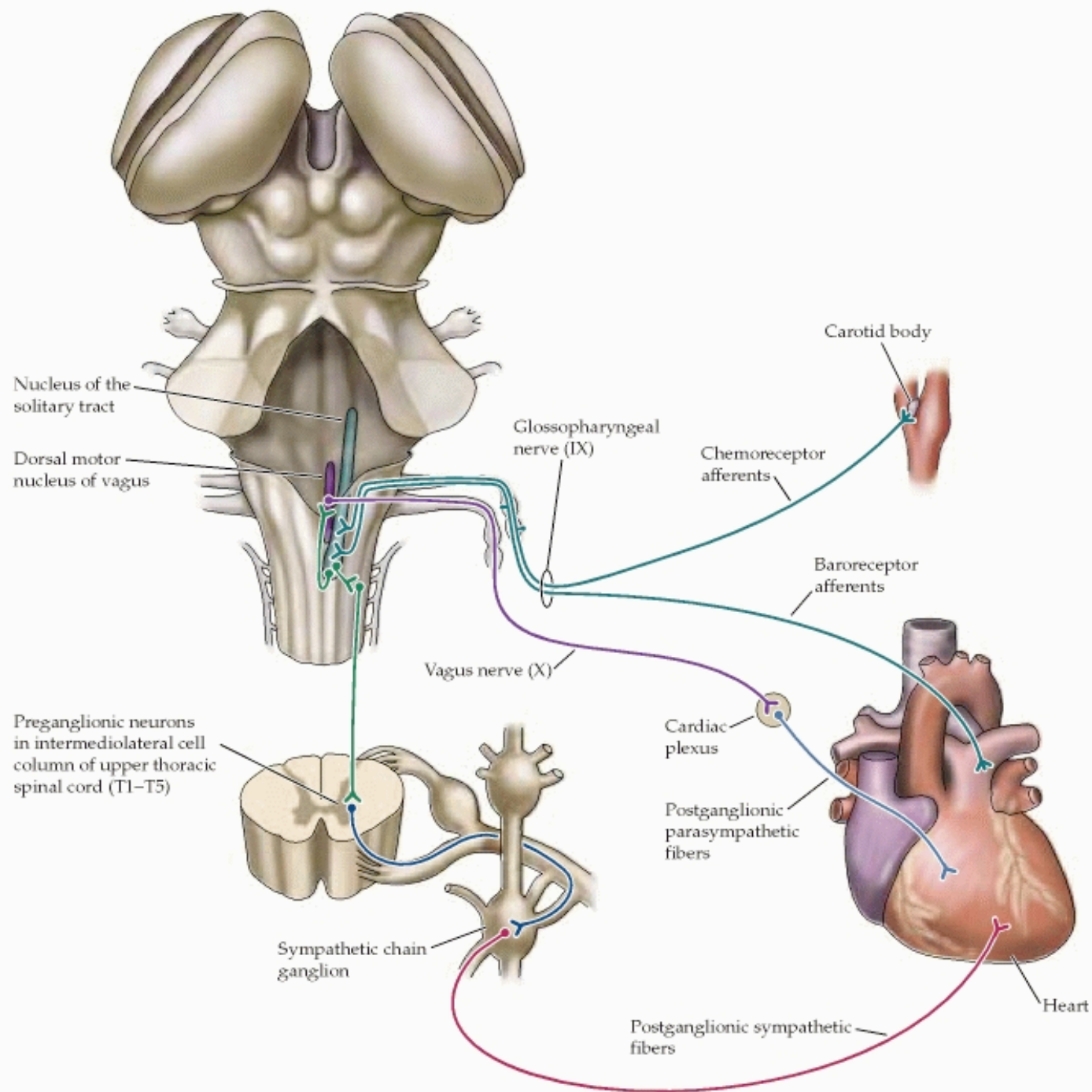
CV Regulation

- **Autonomic regulation**

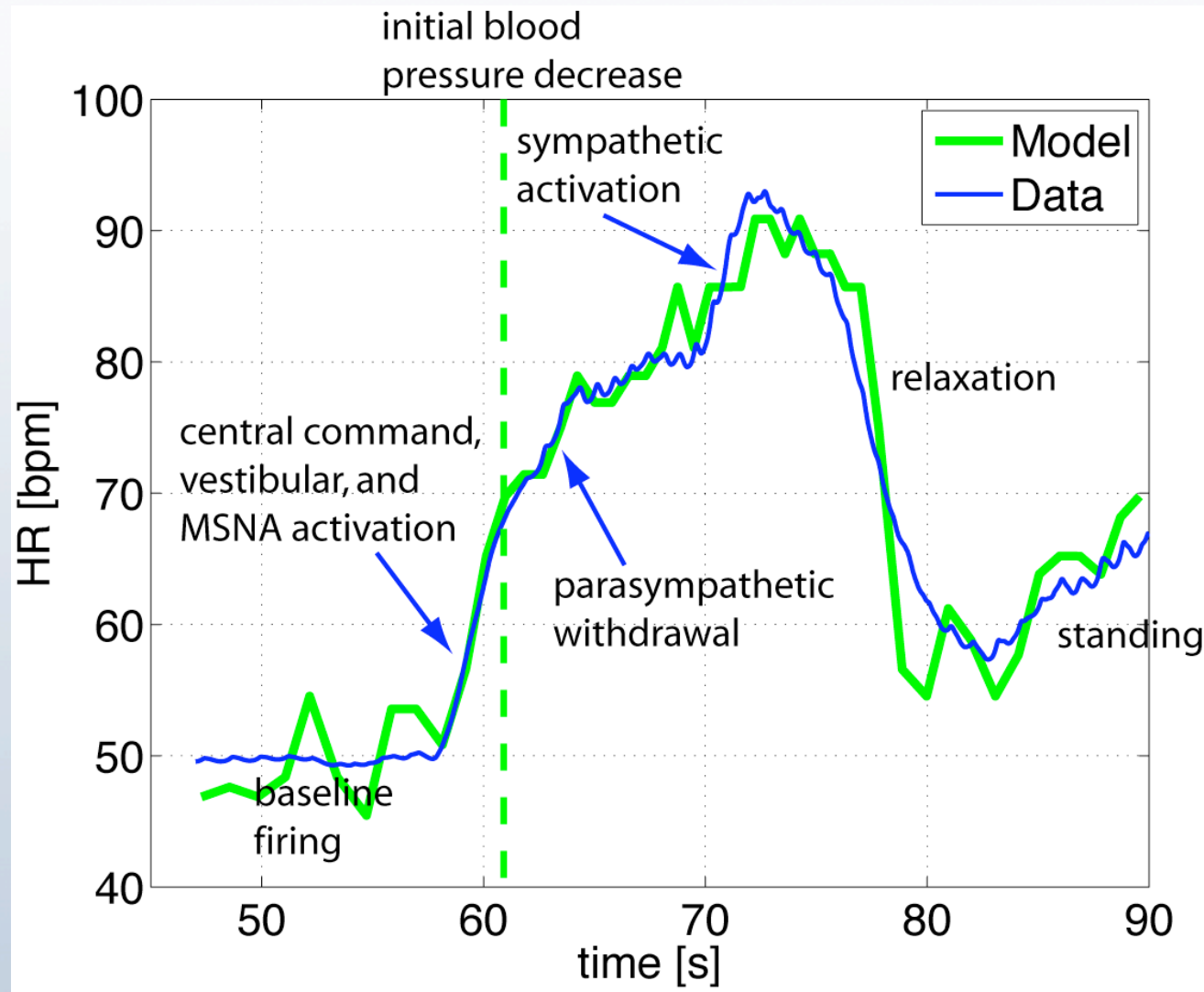
- Mechanical (barosensory) information about pressure in the arterial system
- Chemical (chemosensory) information about the level of oxygen and carbon dioxide in the blood

Parasympathetic and sympathetic activity relevant to CV control is determined by information supplied by these sensors.

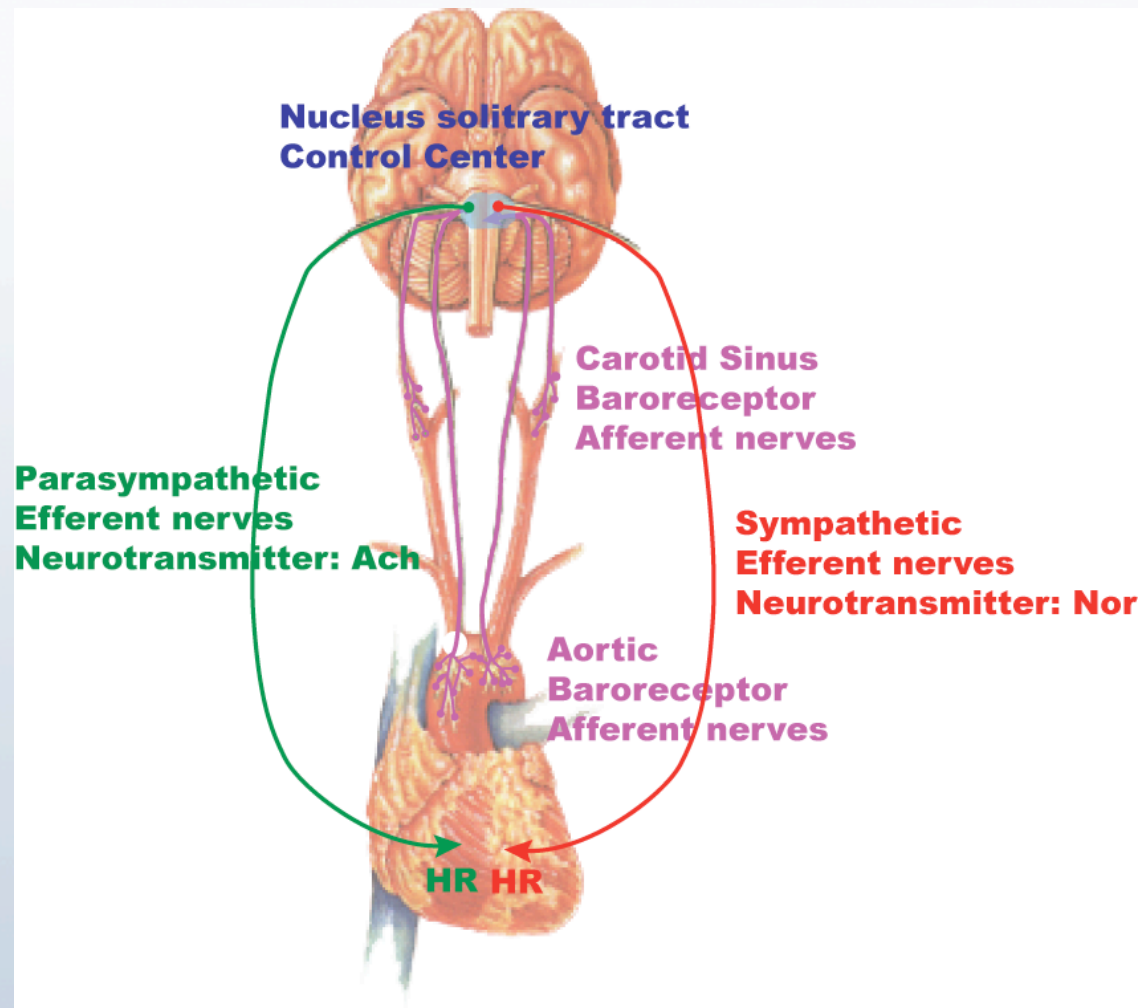
- **Autoregulation** is a process resulting from some internal adaptive mechanism that works to adjust the systems response to stimuli. Prominent in the kidney, the heart, and the brain to maintain perfusion.
- **Hormonal regulation** impact the vasculature in multiple ways: by regulating volume status, modifying smooth muscle contractility directly and through the NO pathway, and by altering cardiac output.



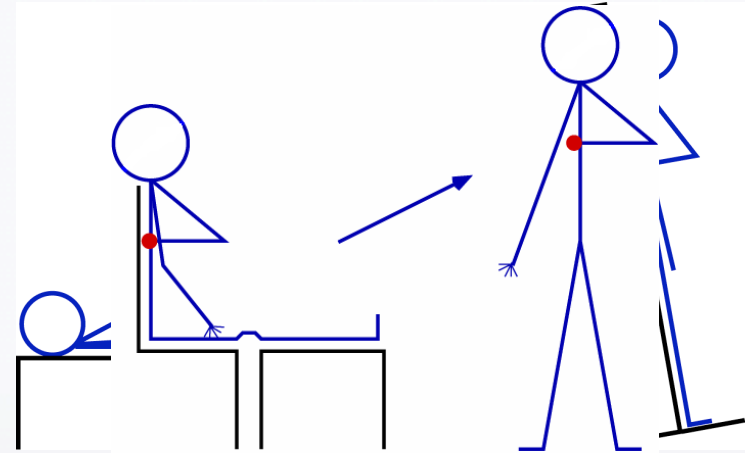
Heart rate regulation (sit-to-stand)



Baroreflex regulation

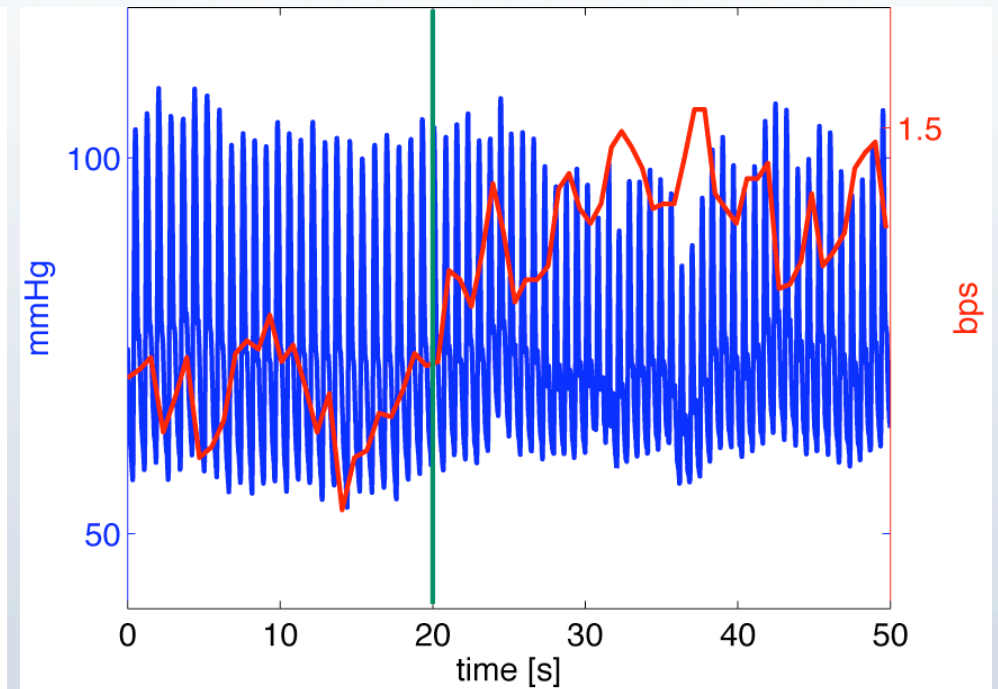
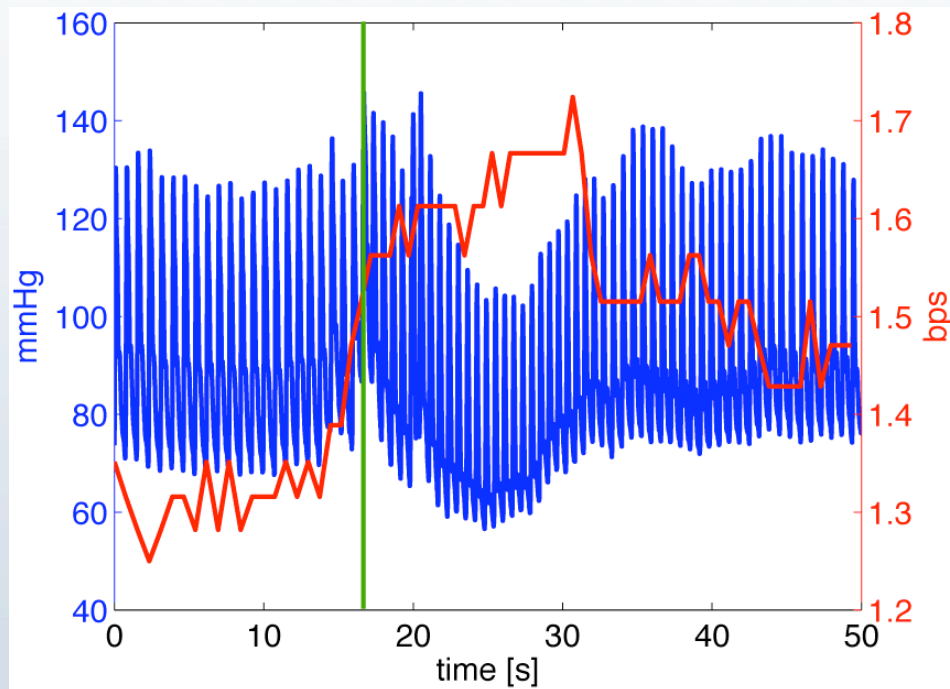


Head-up tilt & Sit-to-stand

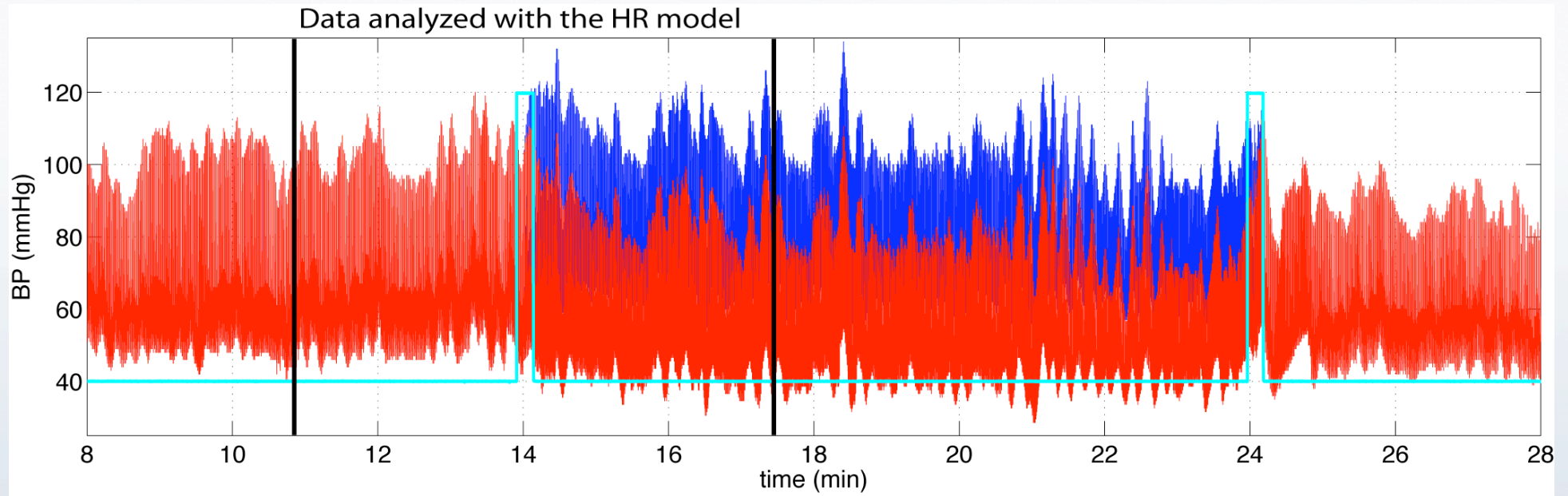


- During head-up tilt blood is pooled in the legs
- As a result, blood pressure in the upper body decreases while pressure in the legs increases
- To bring blood pressure back to homeostasis, heart rate (one of the controlled quantities) is increased

Blood pressure & Heart rate



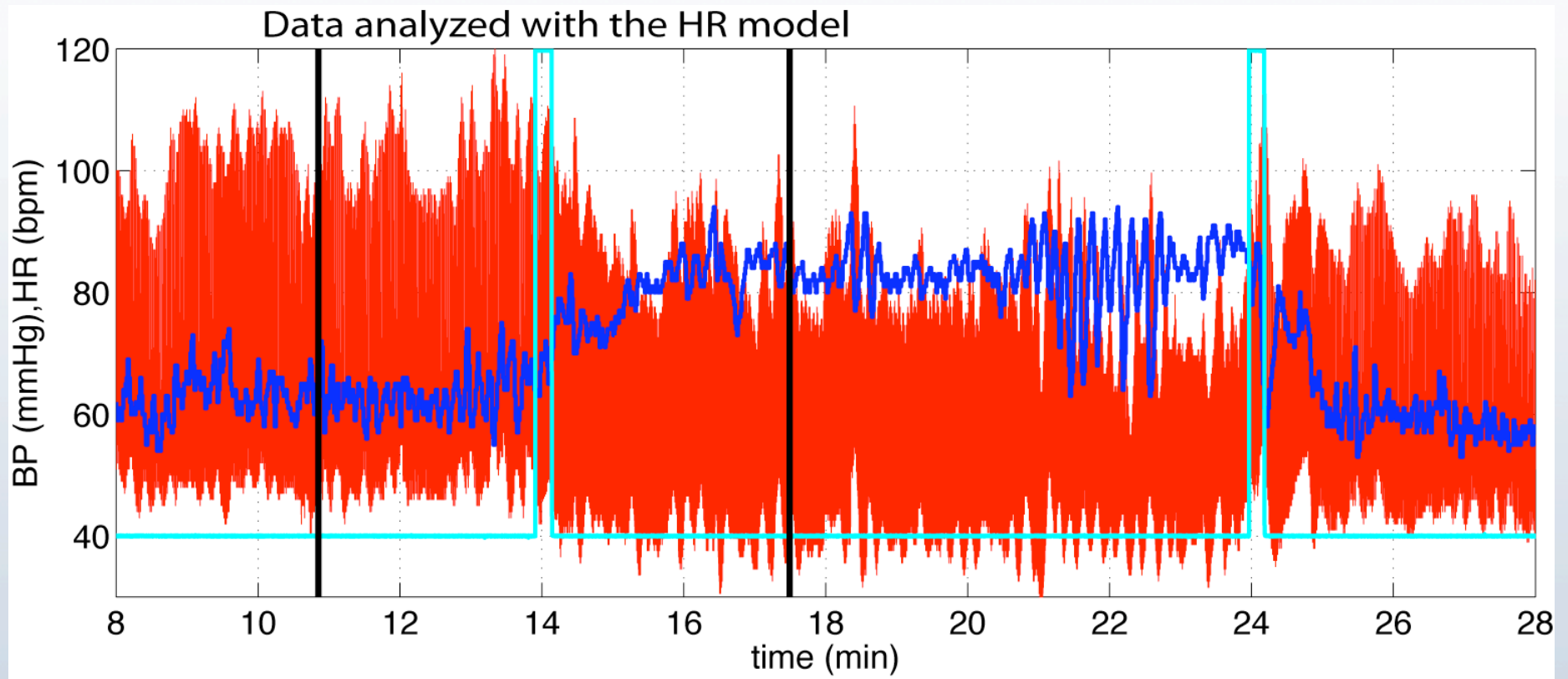
Head-up tilt BP-data



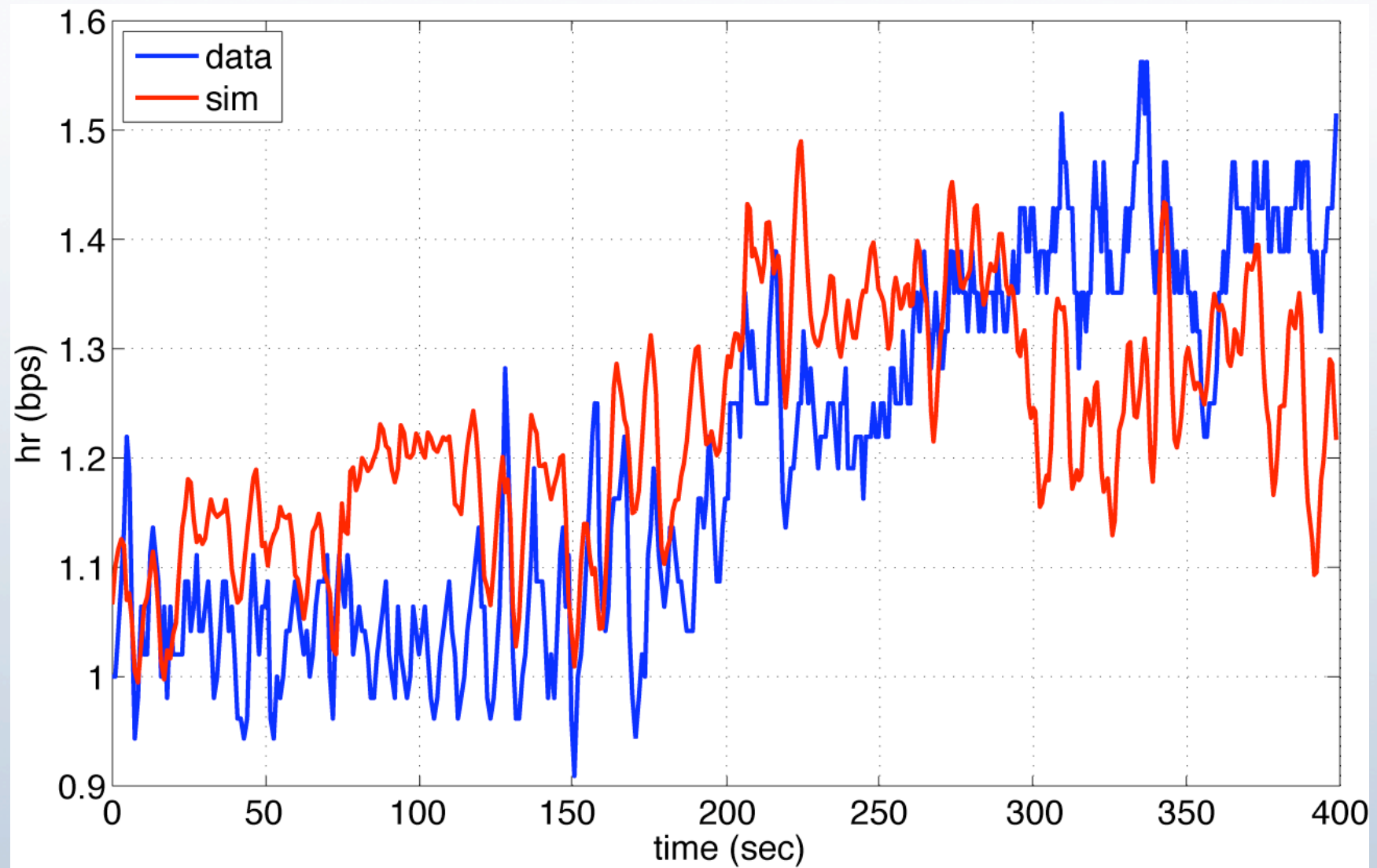
- Finger blood pressure (blue)
- Carotid sinus blood pressure (red)

$$p_{cs}(t) = \rho g h(t), \quad h(t) = \begin{cases} 0 & t \leq t_{st} \\ 60 \frac{t - t_{st}}{t_{ed} - t_{st}} & t_{st} \leq t \leq t_{ed} \\ 60 & t > t_{ed} \end{cases}$$

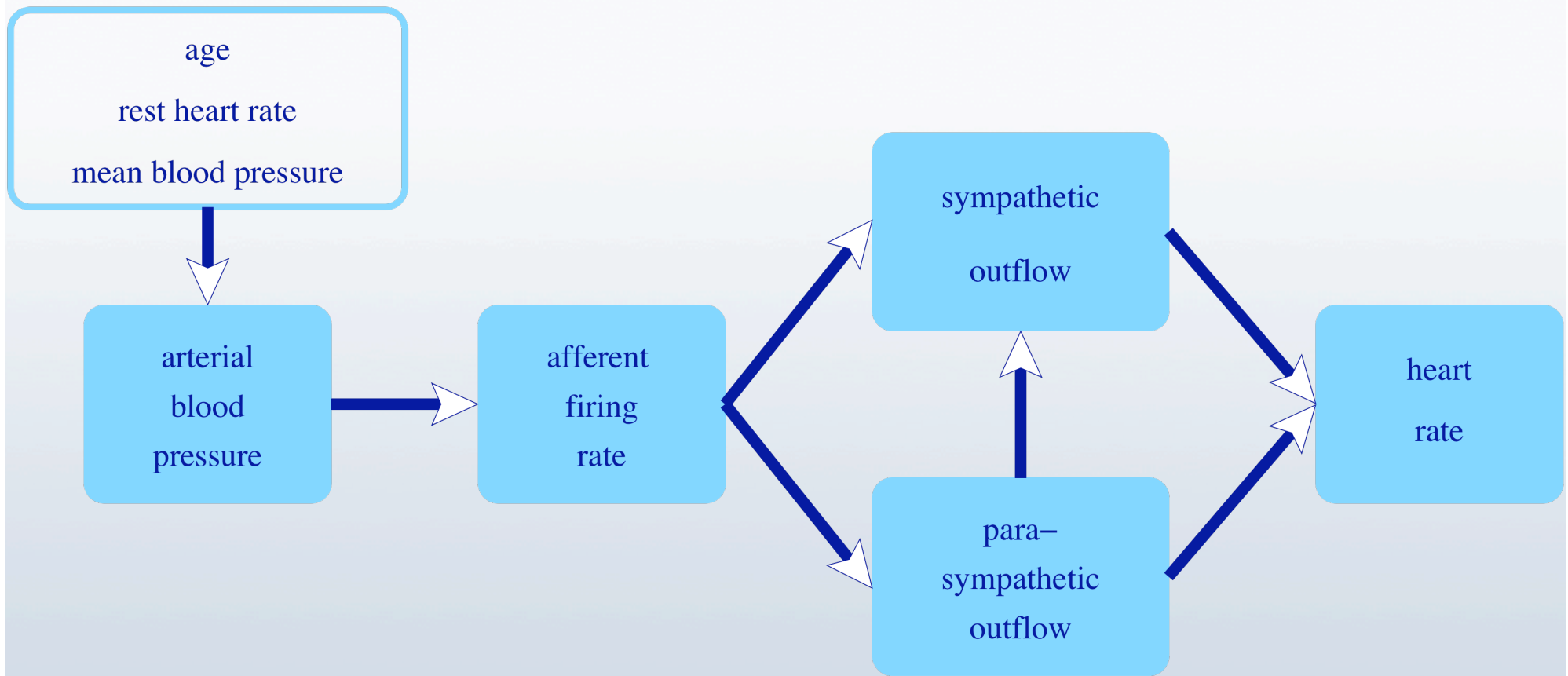
Head-up tilt HR-CBP data



Head-up tilt simulated HR data

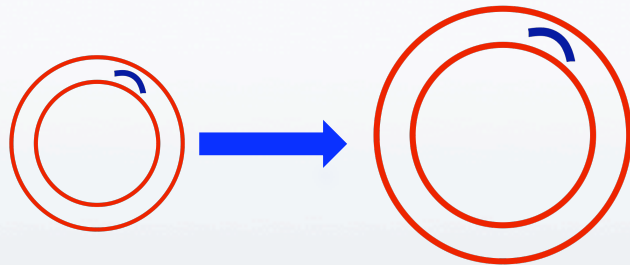


HR model



Baroreceptors

- Stretch receptors sensing stretch of the arterial wall



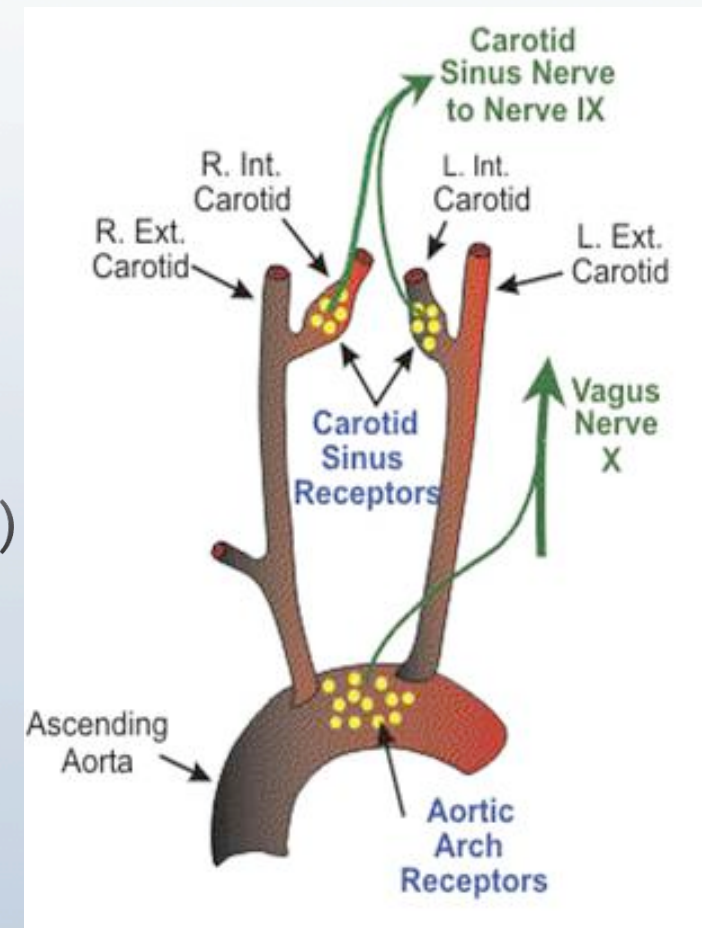
- Stretch proportional to circumference

$$c = 2\pi r$$

$$A = \pi r^2$$

- Blood pressure and area (elastic model)

$$p - p_0 = \frac{Eh}{r_0} \left(1 - \sqrt{\frac{A_0}{A}} \right)$$



Baroreceptors

- Blood pressure and area (viscoelastic models)

$$s(t) = K(0)s^{(e)}[p(t)] + \int_{-\infty}^t K(t - \gamma) \frac{\partial s^{(e)}[p(\gamma)]}{\partial \gamma} d\gamma, \quad s(t) = 1 - \sqrt{\frac{A_0}{A(t)}}$$

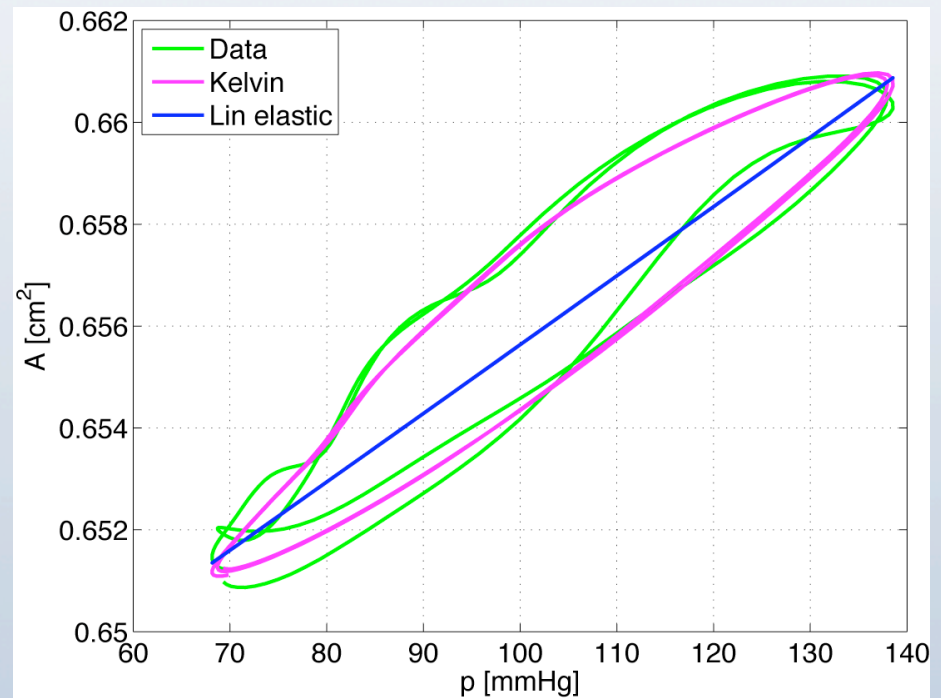
- Kelvin model

$$s^{(e)}[p(t)] = \frac{r_0}{Eh} p(t),$$

$$K(t) = 1 - A_1 e^{-t/b_1}$$

formulated as an ODE

$$s(t) + \tau_{\sigma} \frac{ds}{dt} = \frac{r_0}{Eh} \left(p + \tau_{\epsilon} \frac{dp}{dt} \right)$$

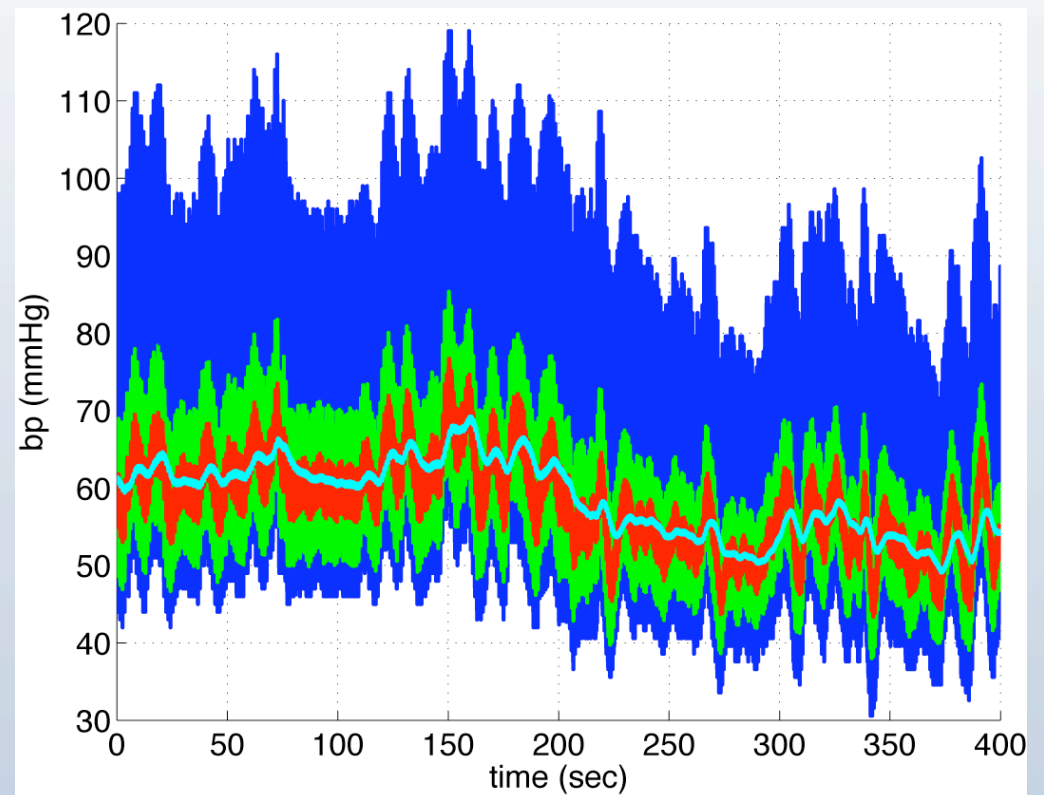
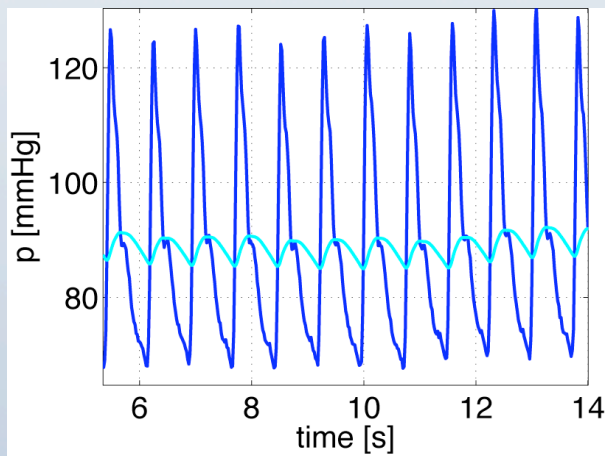


HR model

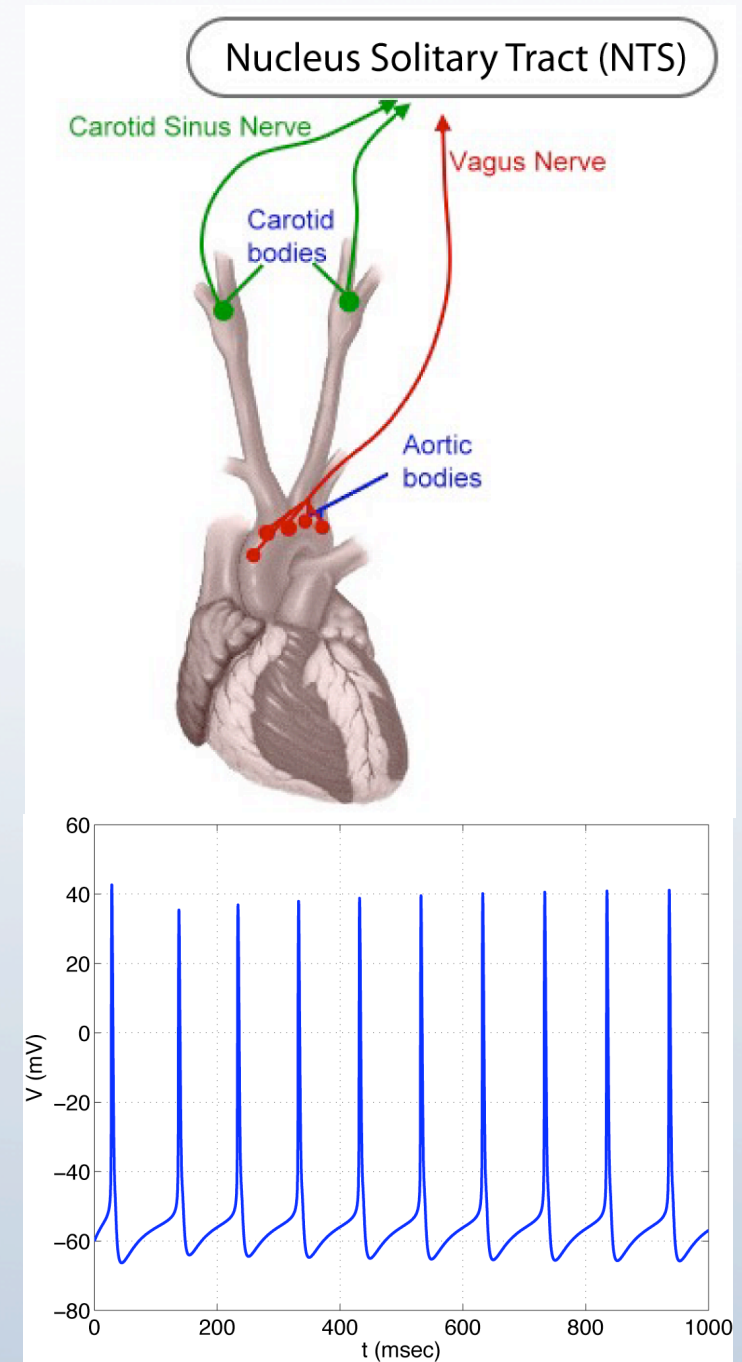
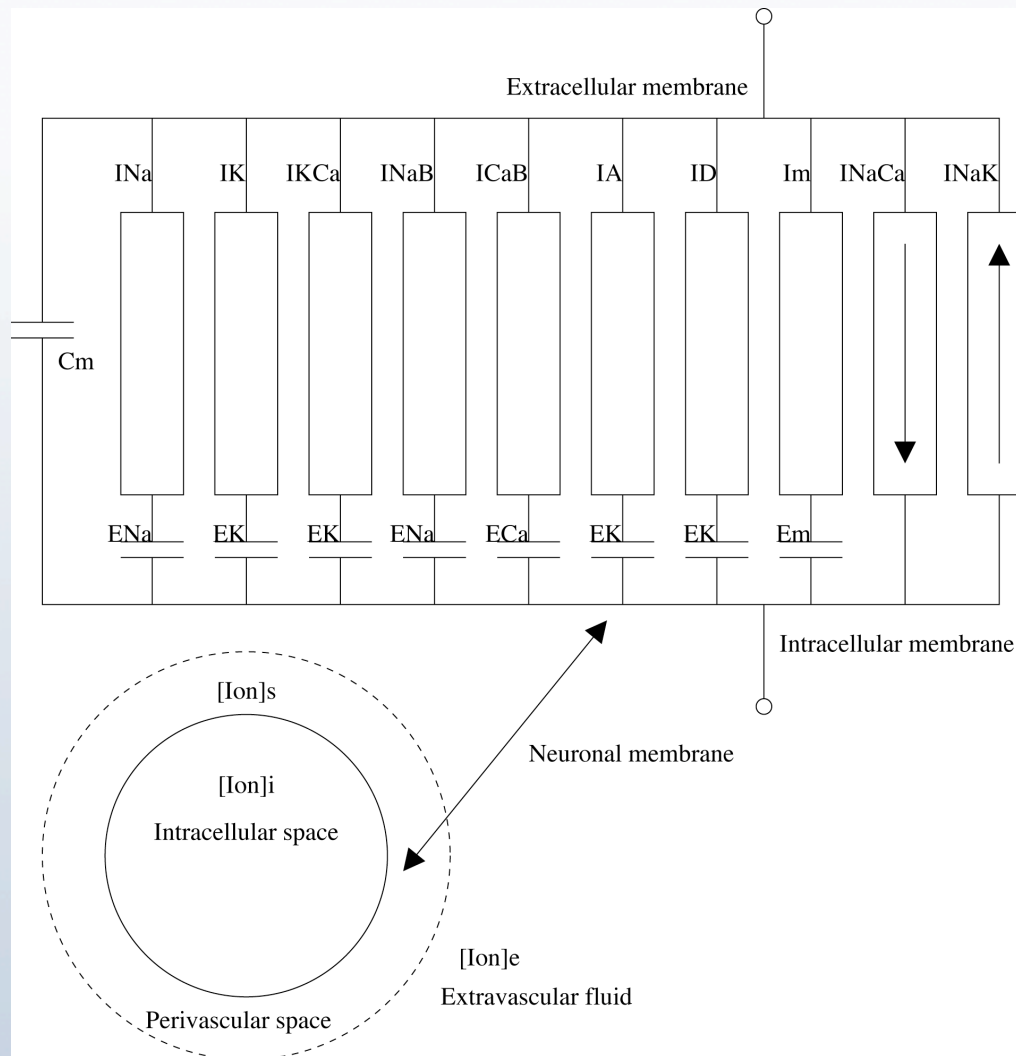
- Running average blood pressure

$$\bar{p}(t) = \alpha \int_{-\infty}^t p(s) e^{-\alpha(t-s)} ds$$

$$\frac{d\bar{p}}{dt} = \alpha(-\bar{p} + p)$$



Afferent firing



Afferent firing

- Membrane voltage

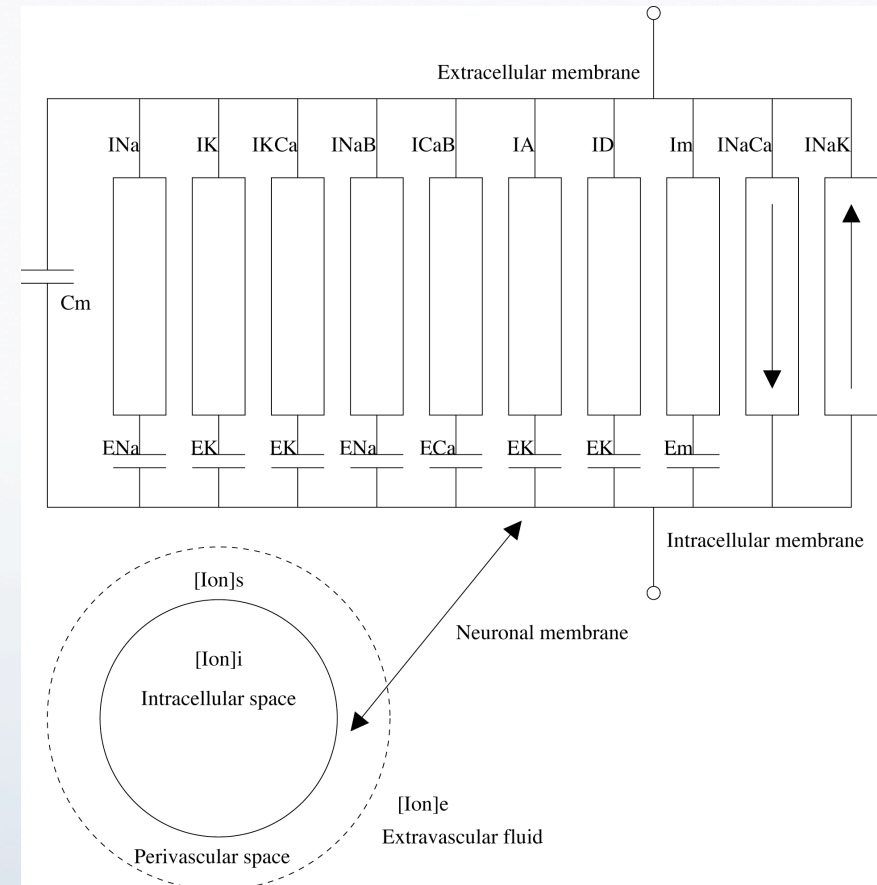
$$\frac{dV}{dt} = \frac{\sum I_{ion} - I_{stim}}{C_m}$$

- Ionic currents

$$I_{ion,i}(t, V) = \bar{g} m_{ion,i}^x h_{ion,i}^y (V - E_{ion,i})$$

$$\frac{dz}{dt} = \frac{z_{\infty} - z}{\tau_z}, \quad z_{\infty}(V) = \frac{1}{1 + \exp\left(\frac{V_{1/2} - V}{S_{1/2}}\right)}$$

$$\tau = A \exp\left[-B^2 (V - V_{peak})^2\right] + C$$



Afferent firing

- Afferent firing rate

$$n(t) = f(V)$$

- Lumped model

$$n(t) = \sum_{i=1}^2 n_i + N$$

$$\frac{dn_i}{dt} = k_i \bar{p} \frac{n(M - n)}{(M / 2)^2} - \frac{n_i}{\tau}, \quad i = 1, 2$$

Sympathetic and parasympathetic outflow

- Sympathetic and parasympathetic outflow

$$\gamma_{par} = \frac{n}{M}$$

$$\gamma_{sym} = \frac{1 - n(t - \tau_d)}{1 + \beta \gamma_{par}}$$

- Neurotransmitters acetylcholine and noradrenaline

$$\frac{dC_{ach}}{dt} = \frac{\gamma_{par} - C_{ach}}{\tau_{ach}}$$

$$\frac{dC_{nor}}{dt} = \frac{\gamma_{sym} - C_{nor}}{\tau_{nor}}$$

- Heart rate

$$h = h_0(1 + m_{nor}C_{nor} - m_{ach}C_{ach})$$

Initial values

- Running average pressure

$$\bar{p}(0) = \text{mean}(P_R)$$

- Afferent firing rate

$$n_1(t) = n_2(t) = 0 \quad \Rightarrow \quad n = N, \quad -\tau_d \leq t \leq 0$$

- Sympathetic and parasympathetic outflow

$$f_{par}(0) = \frac{N}{M}, \quad f_{sym}(t) = \frac{1 - N / M}{1 + \beta N / M}, \quad -\tau_d \leq t \leq 0$$

- Concentrations

$$C_{ach}(0) = f_{par}(0), \quad C_{nor}(t) = f_{sym}(t), \quad -\tau_d \leq t \leq 0$$

- Heart rate

$$h(0) = H_R$$

Parameter values

- Heart rate (beats/min)

- Max heart rate $h_M = 217 - 0.85 \cdot \text{age}$
- Min heart rate $h_m = 30$
- Rest heart rate $h_r = H_R$

- Acetylcholine impact on heart rate

At $h = h_M$ then $n = M$ giving $f_{par} = 1$ and $f_{sym} = 0$ consequently

$$h_M = h_0(1 - m_{ach}) \quad \text{and} \quad m_{ach} = \frac{h_M - h_0}{h_0}$$

- Noradrenaline impact on heart rate

At $h = h_m$ then $n \approx 0$ giving $f_{par} = 0$ and $f_{sym} = 1$ consequently

$$h_m = h_0(1 + m_{nor}) \quad \text{and} \quad m_{nor} = \frac{h_m - h_0}{h_0}$$

Parameter values

- Baseline firing rate N . At $t = 0$

$$h(0) = h_r = H_R = h_0 \left(1 + m_{nor} \frac{1 - N / M}{1 + \beta N / M} - m_{ach} \frac{N}{M} \right)$$

$$N = M \frac{-b + \sqrt{b^2 - 4ac}}{2a}$$

$$a = \beta m_{ach}$$

$$b = \beta(h_r - h_0) / h_0 + m_{nor} + m_{ach}$$

$$c = (h_r - h_0) / h_0 - m_{nor}$$

- Remaining parameters are estimated from literature values.

$$\{\alpha, k_1, k_2, \tau_1, \tau_2, \tau_{ach}, \tau_{nor}, \beta, h_0\}$$

HR model

- Differential equations

$$\frac{dx}{dt} = f(x(t), x(t - \tau_d), t; \theta),$$

$$x = \{\bar{p}, n_1, n_2, C_{ach}, C_{nor}\}$$

- Model output

$$y(t) = g(x(t; \theta), x(t - \tau_d; \theta), t; \theta), \quad y = \{h\}$$

- Output data

$$Y(t_i) = g(x(t_i; \theta), x(t_i - \tau_d; \theta), t_i; \theta) + \varepsilon_i$$

$$Y = \{H\}$$

$$E[\varepsilon_i] = 0, \quad \text{cov}(\varepsilon_i, \varepsilon_j) = 0 \text{ for } i \neq j, \quad \text{var}(\varepsilon_i) = \sigma^2 < \infty$$

HR model

- Model parameters

$$\theta = (\alpha, N, M, k_1, k_2, \tau_1, \tau_2, \tau_{nor}, \tau_{ach}, \beta, h_0, m_{nor}, m_{ach}, \tau_d)^T$$

- Minimization problem

$$\tilde{\theta} = \arg \min_{\theta} J(\theta)$$

$$J(\theta) \approx \sigma^2 = R^T R = \frac{1}{K - q} \sum_{i=1}^K |y(t_i) - Y_i|^2,$$

$$R = (r_1, r_2, \dots, r_K)^T,$$

$$r_i = \frac{y(t_i) - Y_i}{\sqrt{K - q}}$$

Sensitivities

- Classical sensitivity analysis

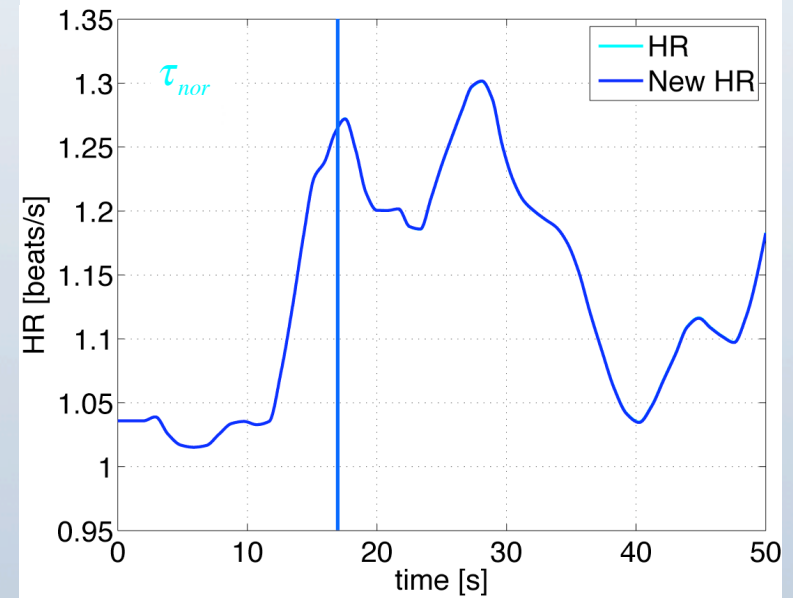
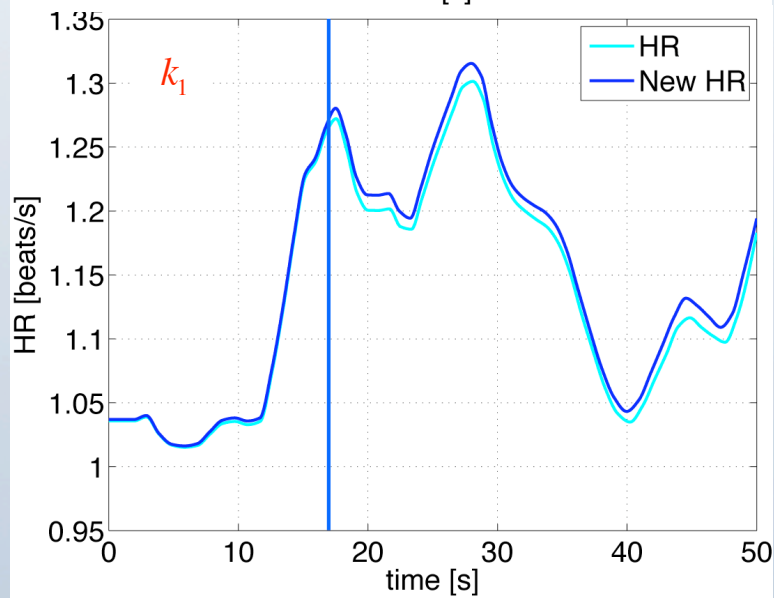
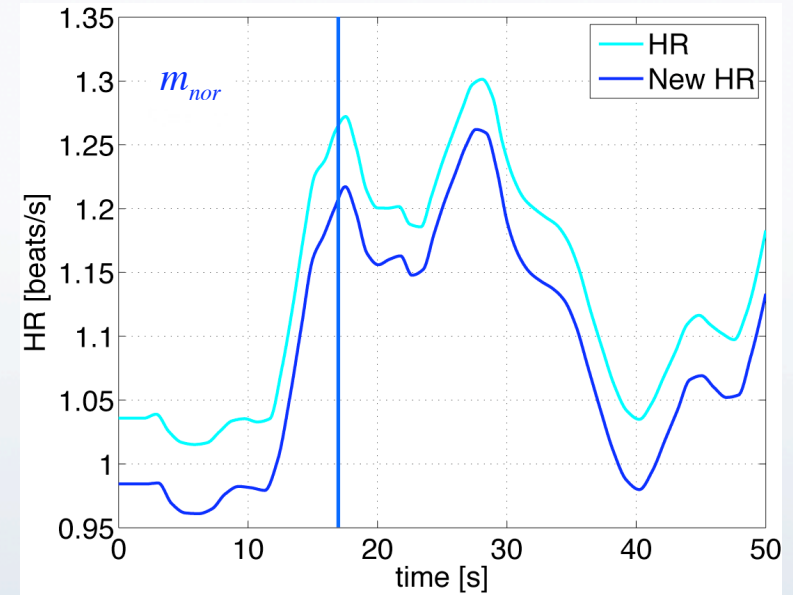
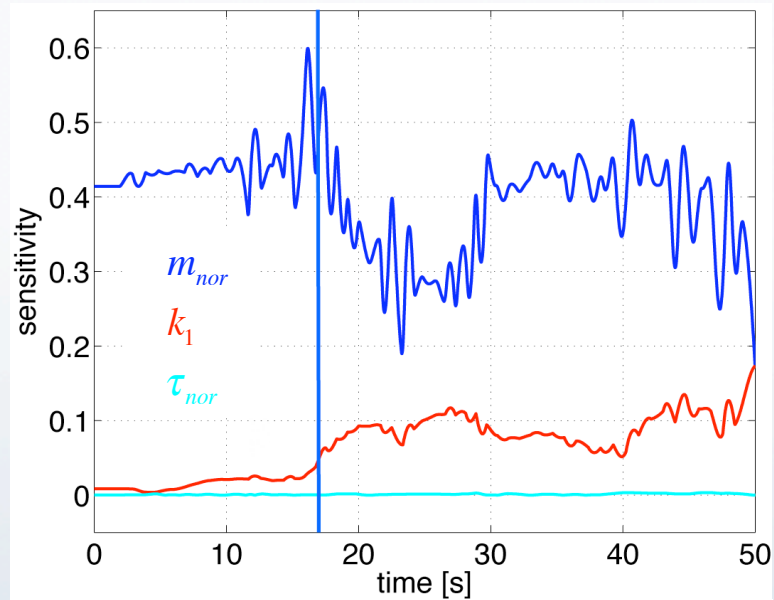
$$S = \frac{\partial y}{\partial \theta} = \frac{\partial y}{\partial x} \frac{\partial x}{\partial \theta} + \frac{\partial y}{\partial x'} \frac{\partial x'}{\partial \theta}, \quad x = x(t), \quad x' = x(t - \tau_d)$$

$$S = \begin{bmatrix} \frac{\partial y(t_1)}{\partial \theta_1} & \dots & \frac{\partial y(t_1)}{\partial \theta_q} \\ \vdots & \ddots & \vdots \\ \frac{\partial y(t_K)}{\partial \theta_1} & \dots & \frac{\partial y(t_K)}{\partial \theta_q} \end{bmatrix}$$

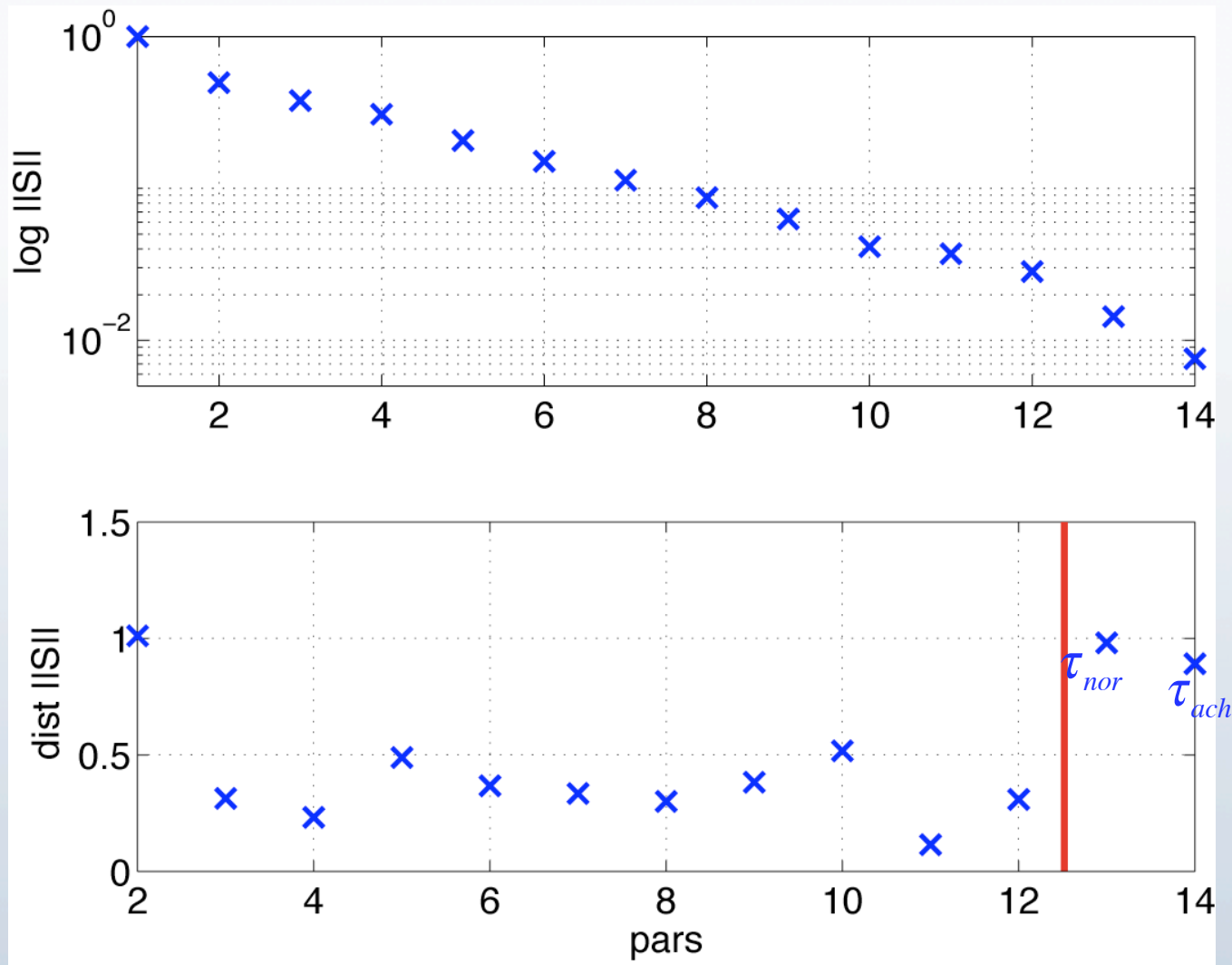
- Ranked sensitivities

$$\tilde{S}_i = \|S_{ij}\| = \{\tilde{S}_{\theta_1}, \tilde{S}_{\theta_2}, \dots, \tilde{S}_{\theta_q}\}$$

Sensitivities



Sensitivities



$$\theta = (\alpha, N, M, k_1, k_2, \tau_1, \tau_2, \beta, h_0, m_{nor}, m_{ach}, \tau_d)^T$$

Subset selection

- Structured correlation analysis
- Singular value decomposition and QR factorization

Structured correlation analysis

- Statistical model

$$Y(t_i) = g(x(t_i; \theta), x(t_i - \tau_d; \theta), t_i; \theta) + \varepsilon_i$$

$$Y = \{H\}$$

$$E[\varepsilon_i] = 0, \text{ cov}(\varepsilon_i, \varepsilon_j) = 0 \text{ for } i \neq j, \text{ var}(\varepsilon_i) = \sigma^2 < \infty$$

- Covariance matrix

$$C = \sigma^2 (S^T S)^{-1}$$

- Correlation matrix

$$c_{ij} = \frac{C_{ij}}{\sqrt{C_{ii} C_{jj}}}, \quad -1 \leq c_{ij} \leq 1, \quad c_{ii} = 1$$

Correlation analysis

	N	k ₁	k ₂	tau ₁	tau ₂	beta	h ₀	m _{nor}	m _{ach}
N	1	-0.29	0.72	0.84	0.04	0.14	-0.52	-0.16	-0.80
k ₁		1	0.12	-0.03	0.61	-0.33	-0.28	-0.27	-0.04
k ₂			1	0.74	0.64	-0.13	-0.91	-0.43	-0.97
tau ₁				1	0.14	0.13	-0.61	-0.14	-0.82
tau ₂					1	-0.35	-0.73	-0.49	-0.54
beta						1	0.09	0.91	-0.02
h ₀							1	0.26	0.90
m _{nor}								1	0.28
m _{ach}									1

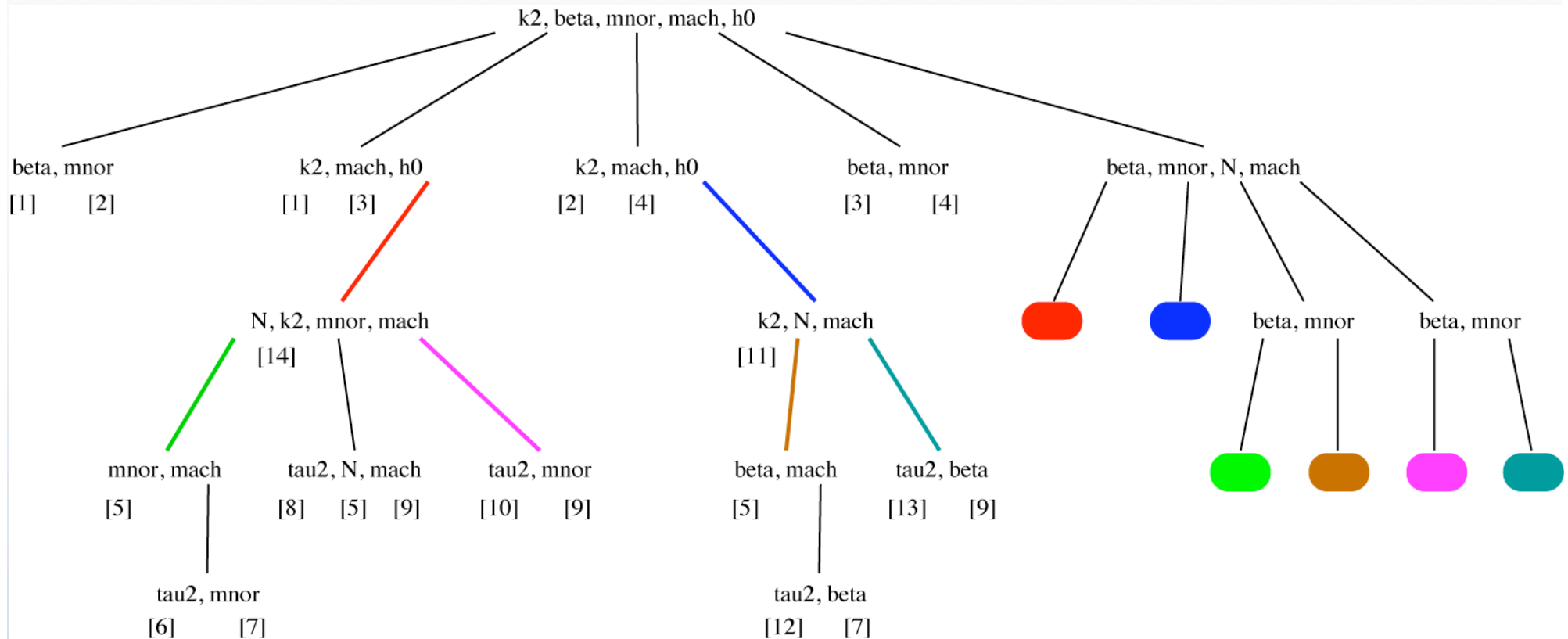
- Correlations: k₂ ~ h₀ ~ m_{ach}, m_{nor} ~ beta
- Sensitivity ranking: k₂, beta, m_{nor}, m_{ach}, h₀
- Fix at *a priori* value: k₂

Correlation analysis

	N	k₁	tau₁	tau₂	beta	h₀	m_{nor}	m_{ach}
N	1	-0.54	0.67	-0.79	0.34	0.46	0.24	-0.64
k₁		1	-0.18	0.71	-0.32	-0.42	-0.25	0.32
tau₁			1	-0.66	0.34	0.24	0.29	-0.62
tau₂					-0.35	-0.45	-0.31	0.47
beta					1	-0.07	0.95	-0.67
h₀						1	-0.33	0.19
m_{nor}							1	-0.66
m_{ach}								1

- Correlations: $m_{nor} \sim \text{beta}$
- Sensitivity ranking: beta, m_{nor}
- Fix at *a priori* value: beta

Subsets via correlations



1: k2, beta

2: k2, mnor [tauA]

3: beta, mach

4: mnor, mach

5: beta, mnor, N, h0

6: tau2, beta, N, mach, h0 [mnor]

7: beta, mnor, N, mach, h0

8: tau2, beta, mnor, h0

9: beta, mnor, mach, h0

10: tau2, beta, mach, h0

11: k2, mnor, h0

12: tau2, mnor, N, mach, h0

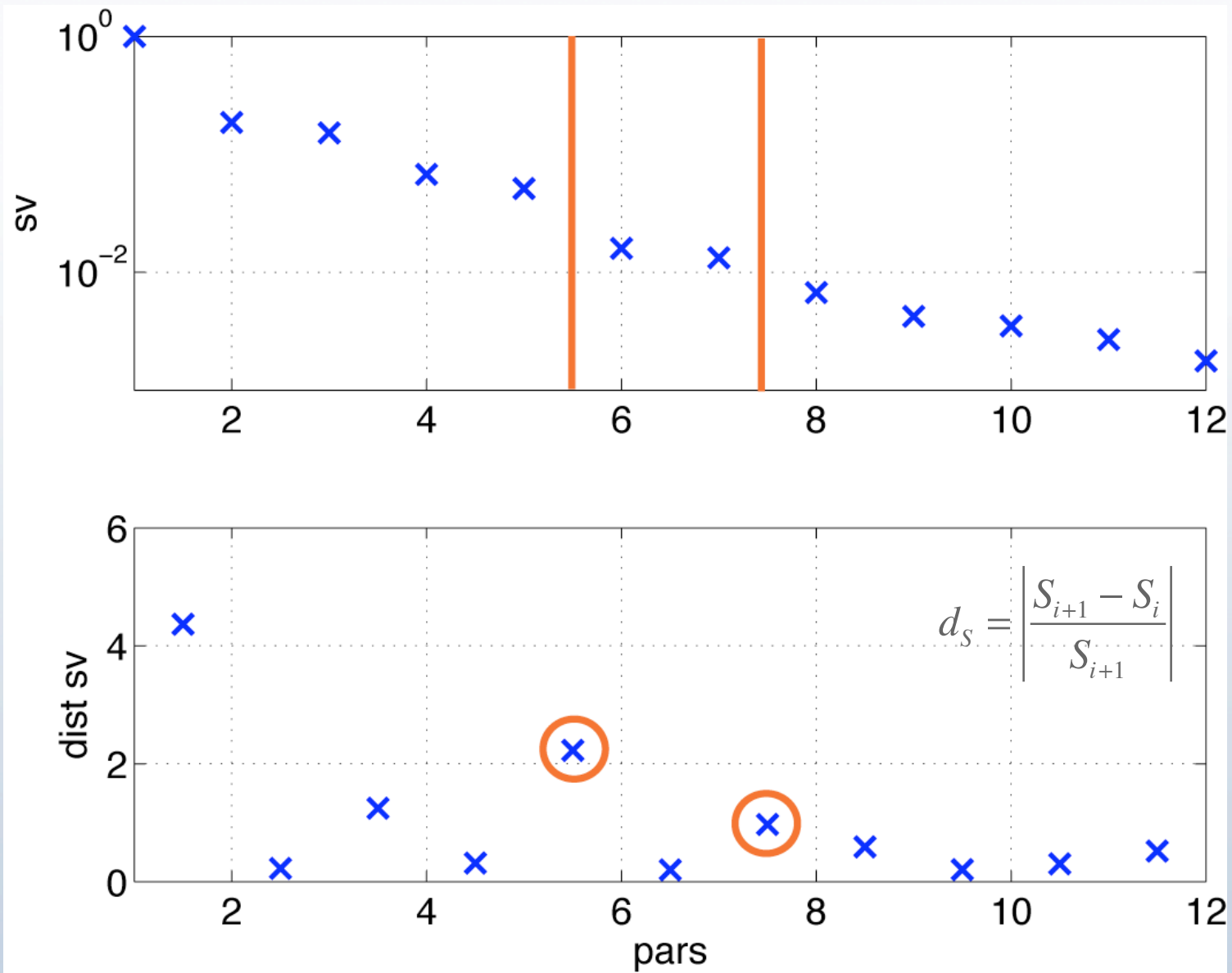
13: tau2, mnor, mach, h0

14: k2, beta, h0 [mnor]

SVD - QR

- The goal of subset selection is to determine the largest set of uncorrelated parameters, that can be estimated given a set of data
- Subset selection via singular value decomposition of the sensitivity matrix $S = \partial h / \partial \theta$
- The numerical rank of the singular values used to estimate the number of parameters included in the subset
 - ✦ Analysis of error bounds: An integration tolerance of 10^{-8} implies that singular values (computed with finite differences) have an accuracy of 10^{-4}
 1. Singular values larger than $10^{-3} \Rightarrow$ All parameters included
 2. Singular values larger than $10^{-2} \Rightarrow$ 6 parameters
 - ✦ Study the relative distance between singular values

SVD - QR



SVD - QR

- Compute S and rewrite $S = U \Sigma V^T$, where the singular values $\text{diag}(\Sigma)$ are sorted from the largest to smallest
- Determine the numerical rank ρ of S
- Partition the matrix of eigenvectors $V = [V_\rho \ V_{n-\rho}]$
- Determine a permutation matrix P by constructing a QR decomposition with column pivoting, i.e., determine P such that $V_\rho^T P = QR$
- Use P to reorder the parameter vector as $\hat{\theta}_0 = P^T \theta_0$
- Make the partition $\hat{\theta}_0 = [\hat{\theta}_{0,\rho} \ \hat{\theta}_{0,n-\rho}]$
- Fix $\hat{\theta}_{n-\rho}$ at the a priori estimates $\hat{\theta}_{0,n-\rho}$
- The subset of identifiable parameters contains $\hat{\theta}_\rho$

Parameter estimation

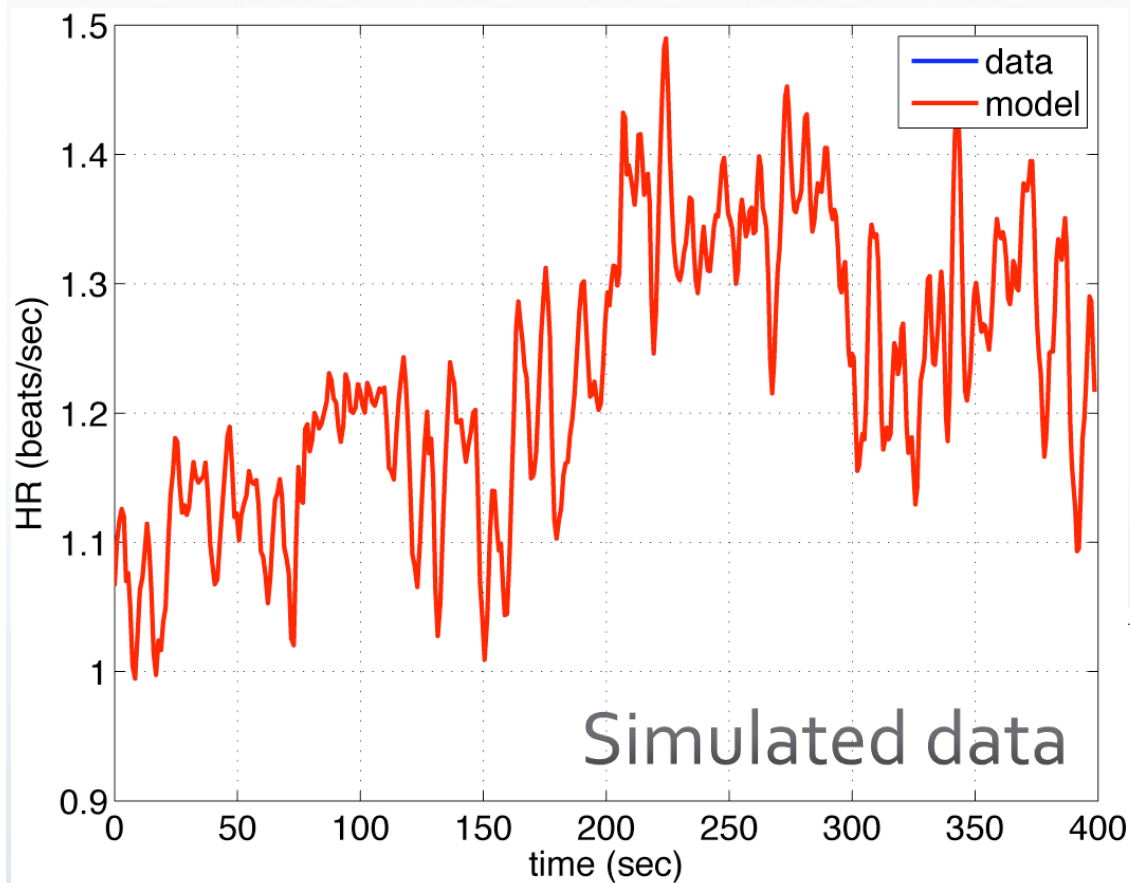
- For each subset of parameters, values were estimated using the Levenberg-Marquart method to solve the minimization problem

$$\tilde{\theta} = \arg \min_{\theta} J(\theta)$$

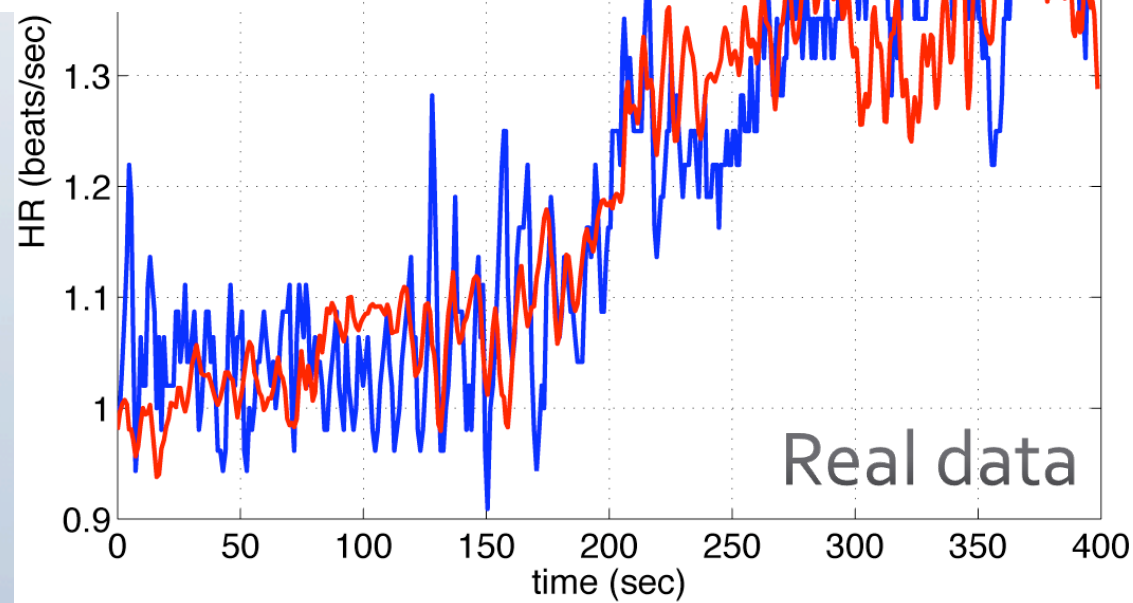
$$J(\theta) \approx \sigma^2 = R^T R = \frac{1}{K - q} \sum_{i=1}^K |y(t_i) - Y_i|^2,$$

$$R = (r_1, r_2, \dots, r_K)^T,$$

$$r_i = \frac{y(t_i) - Y_i}{\sqrt{K - q}}$$



Results



Akaike information criterion

- To compare results for each subset we used the Akaike information criterion, which for least squares problems can be formulated as

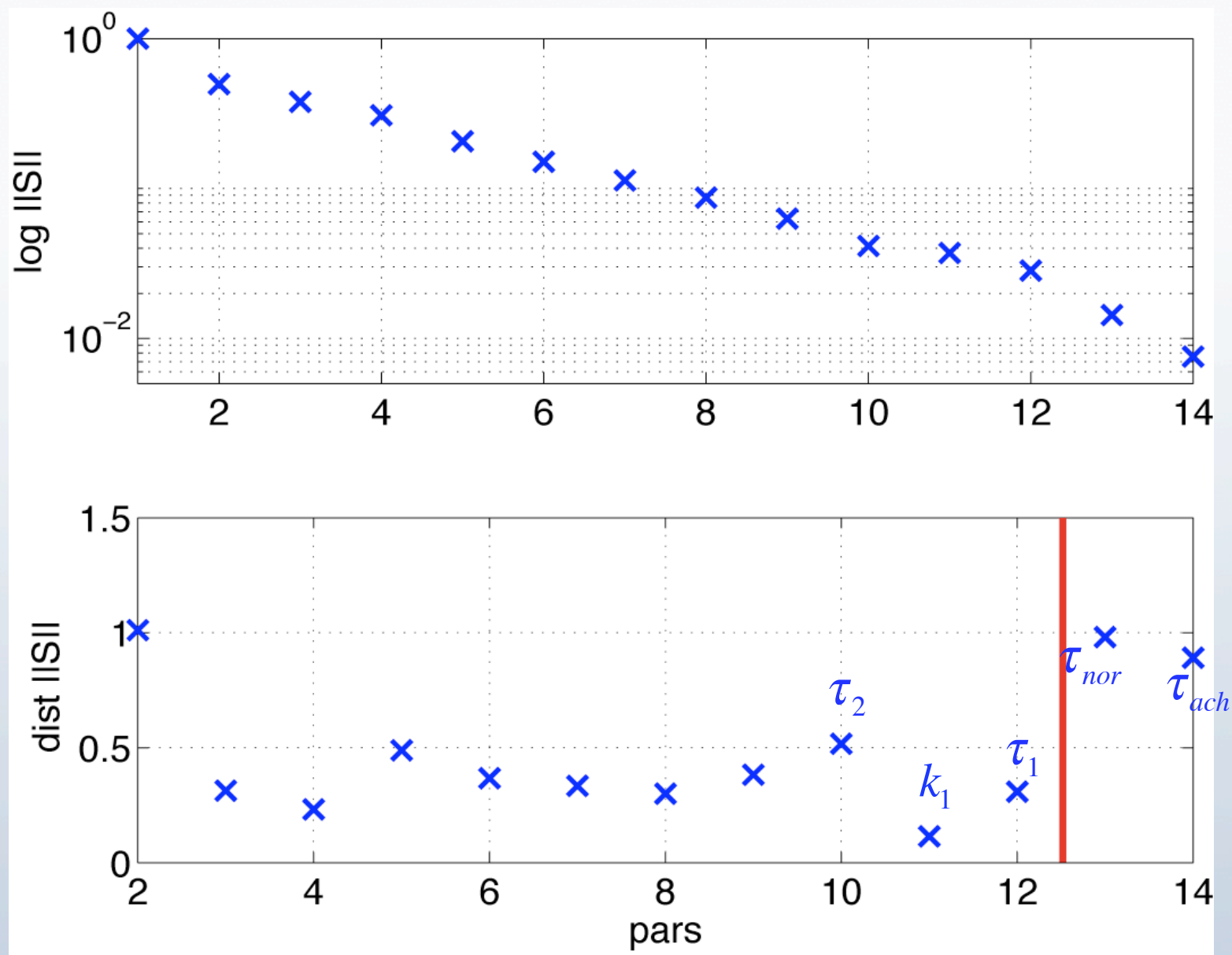
$$AIC = K \log J + 2q$$

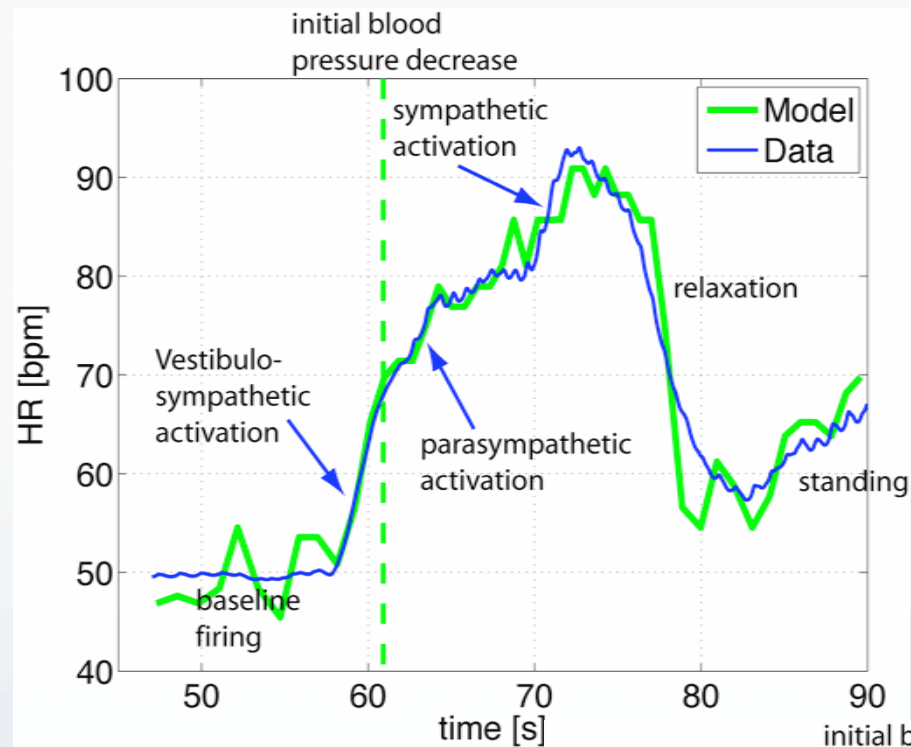
J is the least squares cost

K is the number of samples in the timeseries

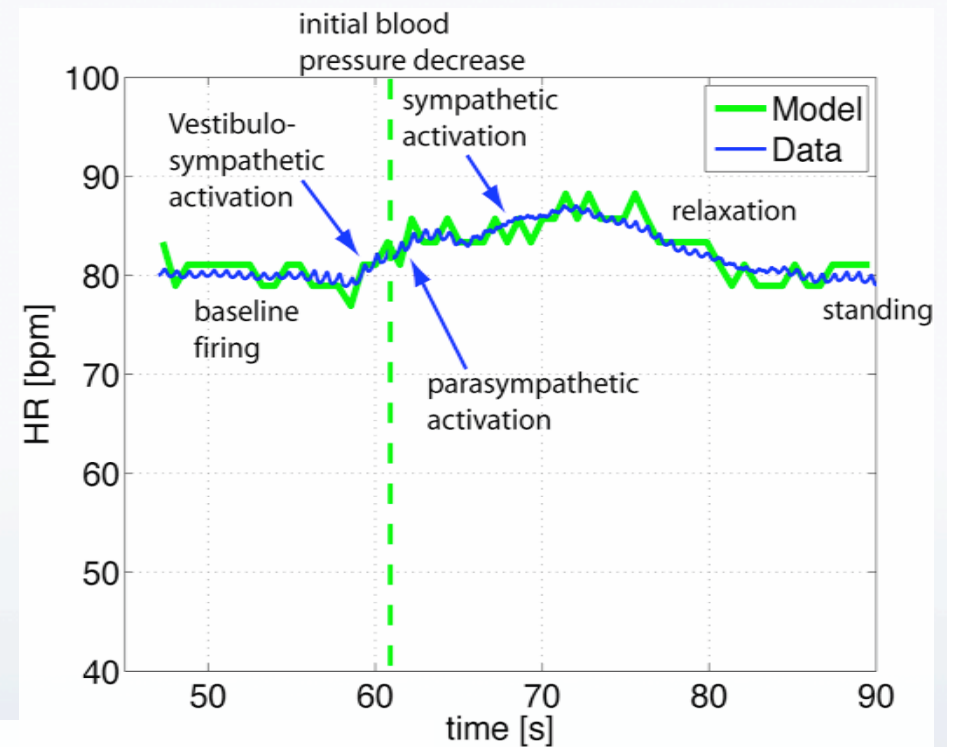
q is the number of model parameters

Subsets						Grad	J	par	norm	cor	AIC	Rank
SVD-QR												
2	4	5	11	13		7.9e-5	7.1e-7	k2	6.68	5,11,13	-6.77	18
2	4	5	11	12	13	8.6e-5	8.0e-7	mnor	14.7	5,13	-6.71	19
Correlation analysis												
2	4	6	7	11	12 13	4.9e-5	1.5e-8	mnor	4.28	none	-8.61	5
2	4	5	6	7	11 12	2.0e-5	1.0e-8	k1	2.08	NA	-8.81	3
2	4	6	7	11	12 13	4.9e-5	1.5e-8	msym	4.28	NA	-8.61	5
2	4	5	6	7	10 11	8.5e-5	3.0e-8	k1	3.03	NA	-8.29	7
2	4	6	7	10	11 13	7.8e-5	6.4e-6	k1	47.6	NA	-5.71	21
2	4	7	10	11	13	3.5e-5	3.5e-9	k1	0.86	NA	-9.31	1
2	4	6	7	10	13	1.7e-5	9.7e-9	tau1	1.37	NA	-8.83	2
2	4	6	7	12	13	5.4e-5	2.1e-7	mnor	30.1	NA	-7.35	14
2	4	6	7	13		2.5e-5	1.6e-8	tau1	1.53	NA	-8.60	6
2	4	5	6	12		4.4e-5	8.5e-8	k1	2.25	NA	-7.79	9
2	4	5	6	7		6.2e-5	8.6e-8	k1	1.84	NA	-7.79	10
2	4	5	6	13		6.1e-5	1.7e-e7	k1	2.89	NA	-7.45	11
2	4	5	6	10		7.0e-5	2.4e-e7	k1	2.31	NA	-7.30	15
4	5	6	7	13		9.9e-5	1.3e-6	k1	9.99	NA	-6.48	20
4	5	6	10			4.1e-5	8.0e-8	k1	1.55	NA	-7.82	8
4	5	6	7			4.5e-5	2.4e-7	k1	2.25	NA	-7.29	16
4	5	6	12			6.1e-5	2.9e-7	msym	11.99	NA	-7.21	17

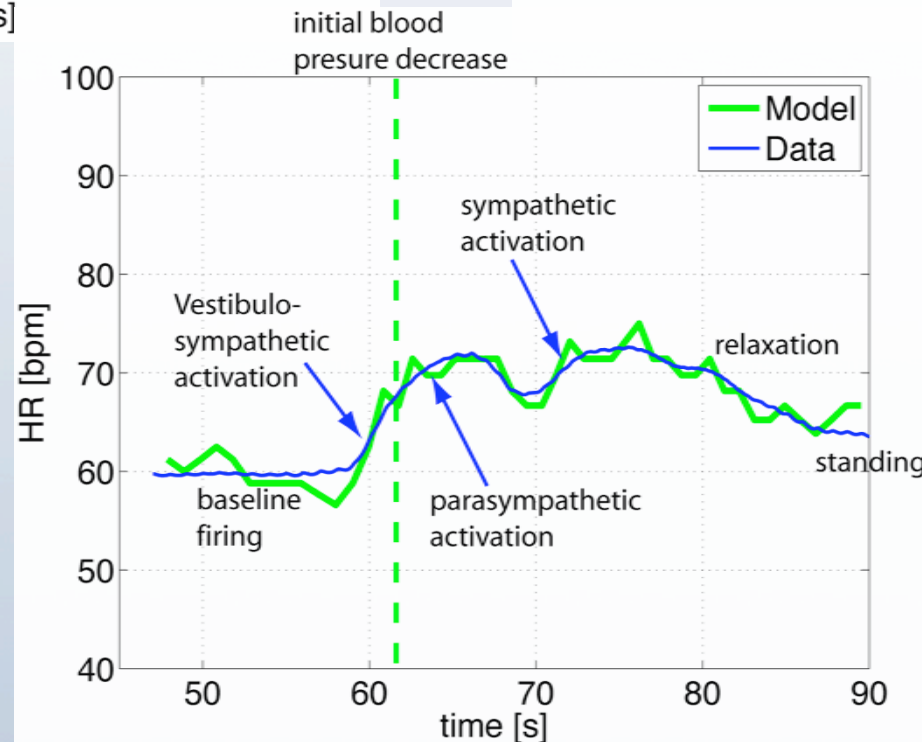




Healthy young subject

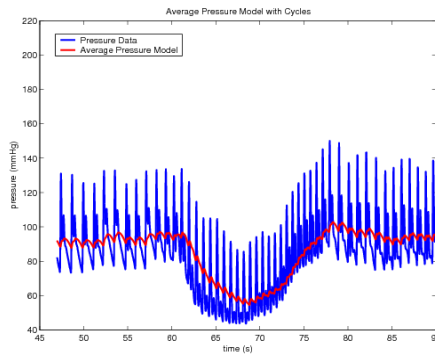


Hypertensive elderly subject

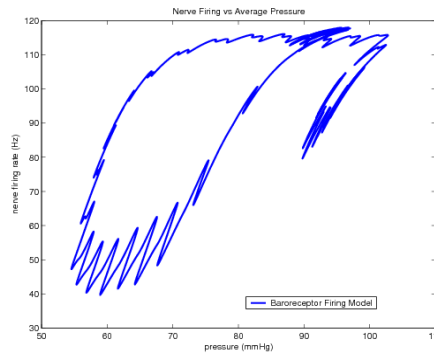


Healthy elderly subject

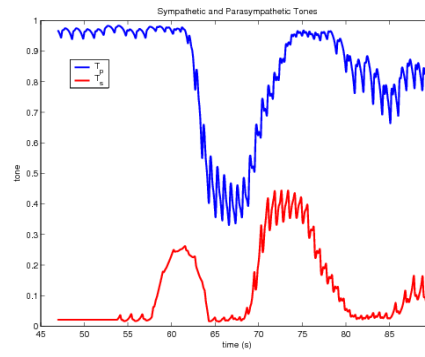
**Healthy
young
subject**



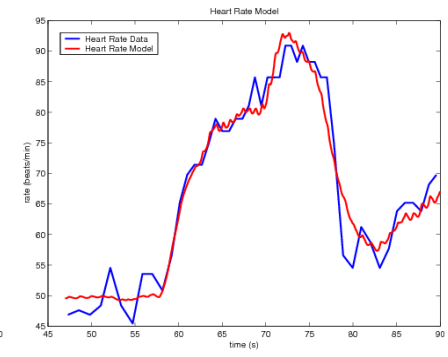
Pressure (blue, data) and mean pressure (red) vs. time



Firing rate vs. pressure (hysteresis loop is wide and closed)

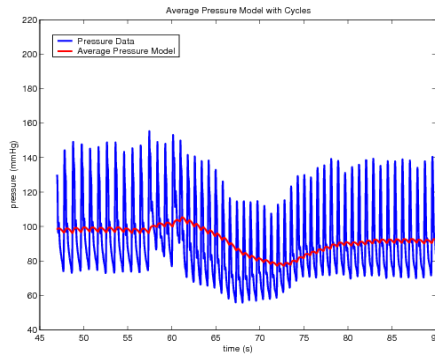


Parasympathetic (blue) and sympathetic (red) tones vs. Time:

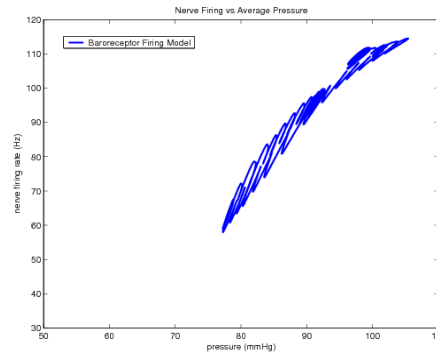


HR data (blue, data) and HR model (red) vs. time

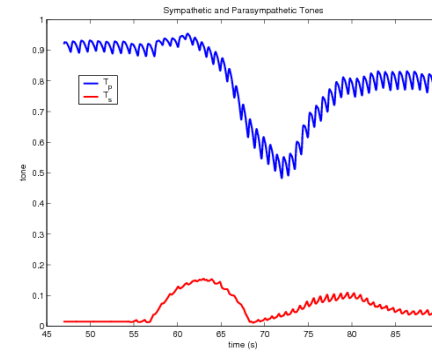
**Healthy
elderly
subject**



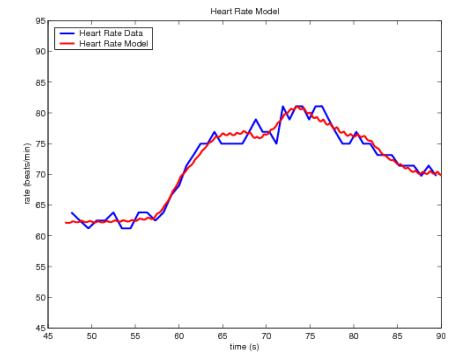
Reduced dynamics and lower resting state



Loop narrow with decreased slope; indicates reduced dynamics

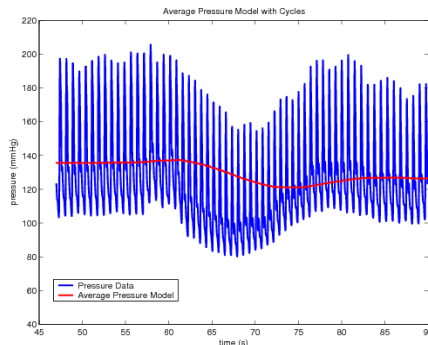


Diminished tone, in particularly sympathetic tone

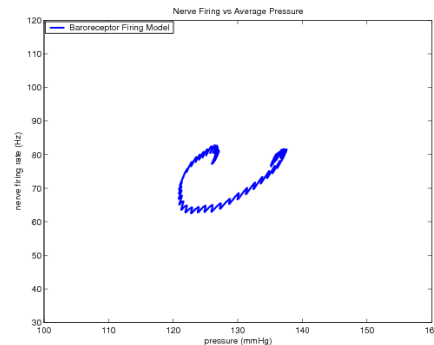


Reduced dynamics, higher resting state, slower regulation

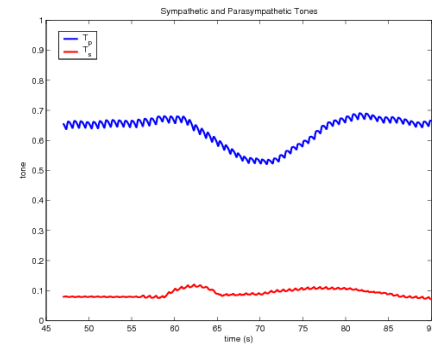
**Hypertensive
elderly
subject**



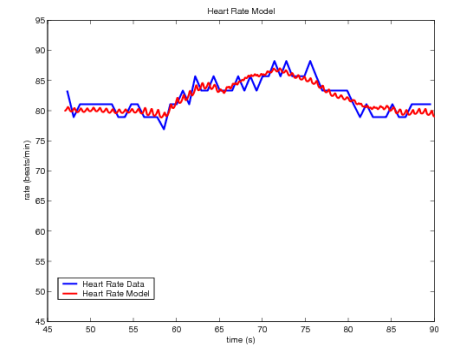
Reduced dynamics and longer regulation timescale



Reduced dynamics, not returning to steady state

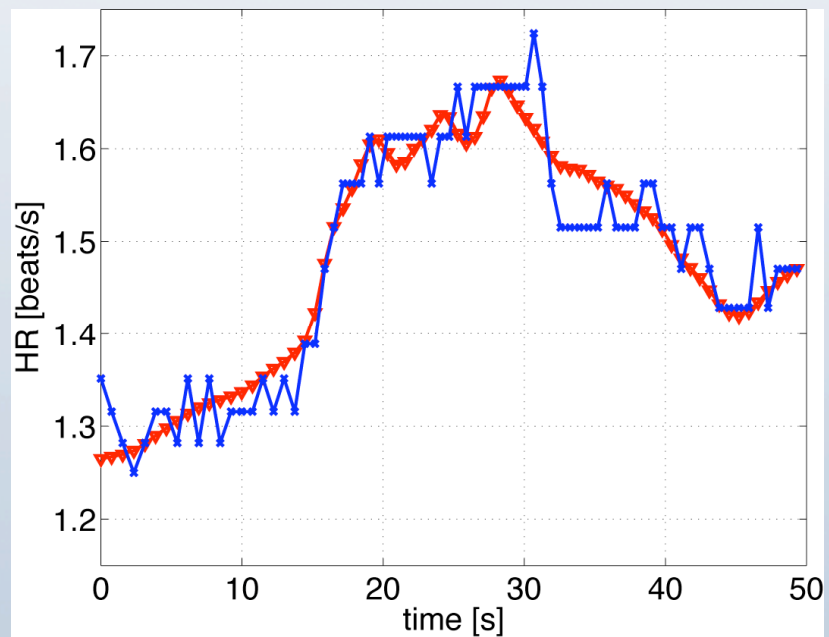
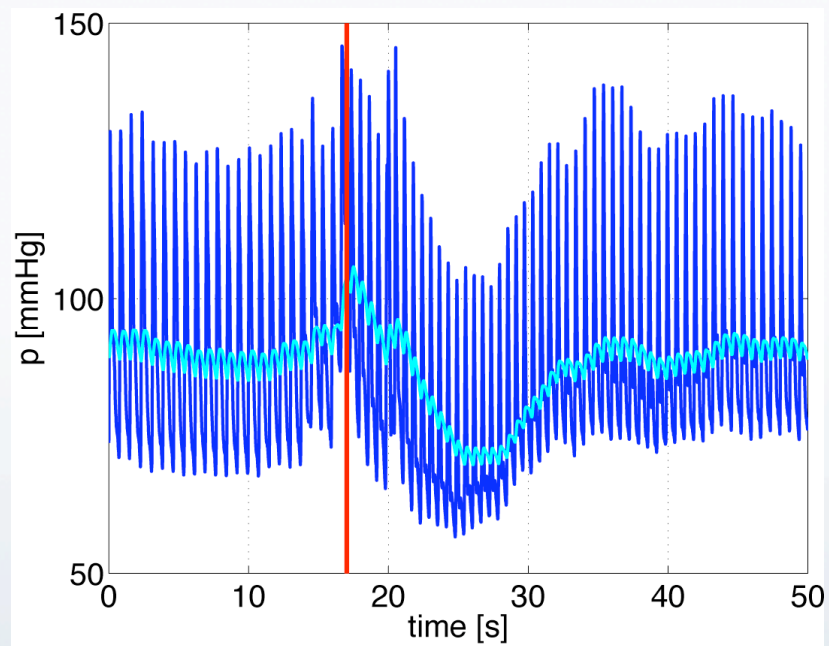


Significant sympathetic reduction

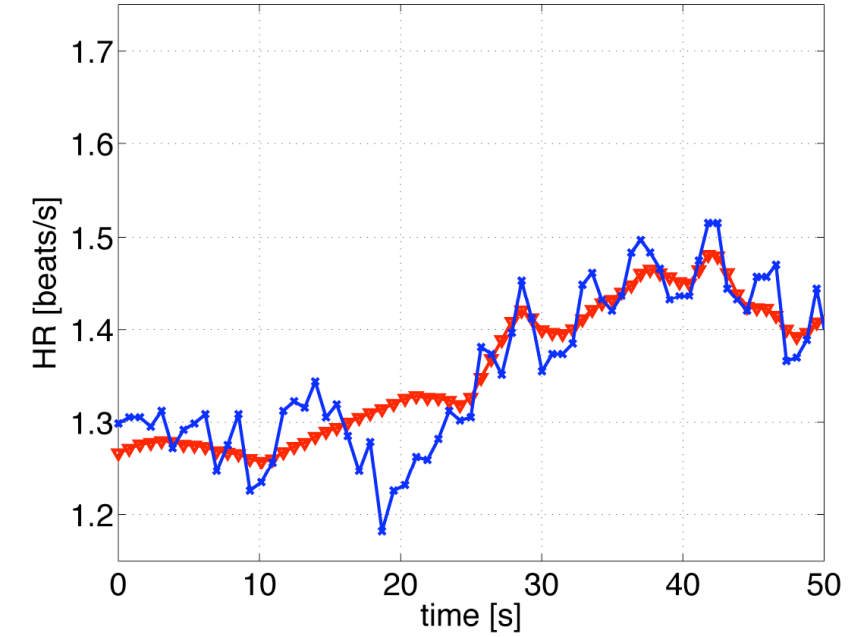
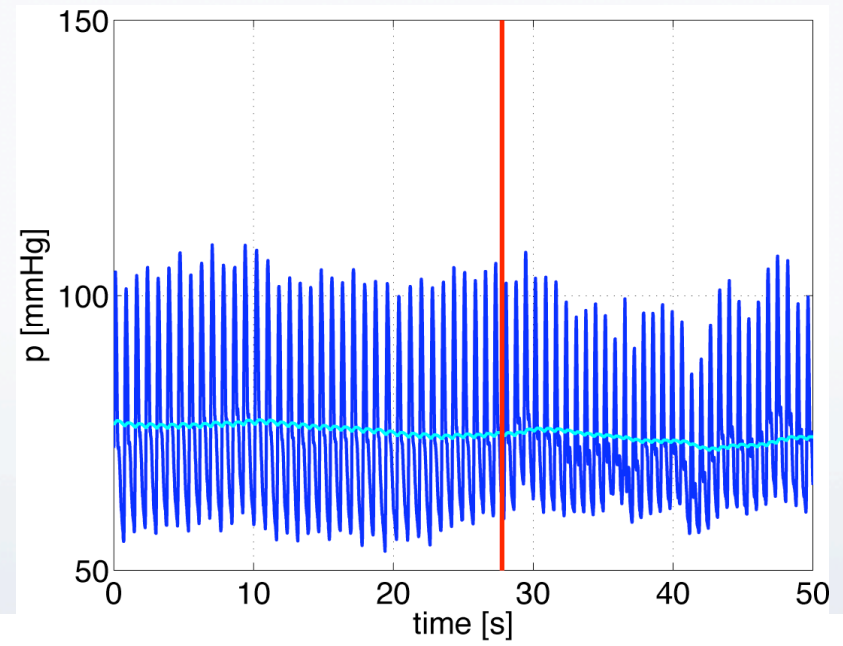


Reduced dynamics, higher rest state, slower regulation

Sit-to-stand



Head-up-tilt



Discussion

- Estimation of all model parameters often leads to unreliable parameter estimates, in particular if the parameter set includes insensitive and correlated parameters
- Subset selection methods improves identifiability of parameters
- Numerous subset selection methods exists including Kalman filtering, principal component analysis, SVD-QR factorization and/or correlation analysis
- Physiological/biological considerations should be done as well to ensure estimation of parameters that have relevance for the user

Discussion

- Structured correlation analysis performs “better” than SVD-QR, the AIC values are lower
- The “winner” subset is more stable to perturbations in initial parameter values
- Note SVD-QR subsets still contain correlated parameters
- Note parameters with the largest error are always the least sensitive parameters left in the set

Discussion

- Correlation analysis is more time consuming to perform
- If analysis is performed with initial parameters far from the true parameters, the analysis should be repeated for a sweep of parameters using a Monte-Carlo type approach
- Methods could be combined using an iterative approach
- If the model is not correct, these methods do not perform well and parameter estimation methods do not converge even with a reduced parameter set

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