Dosimetry of double orbit cone beam computed tomography (CT) as applied to image guided radiotherapy (IGRT)

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IGRT: current status



Varian Trilogy linear accelerator with integrated on-board imager
Efficient imaging systems allow for precise delivery of radiation treatment

 On Board Cone Beam CT is a relatively new development in image guided radiotherapy

Cone beam CT (CBCT)





- Pulses of low energy kV x-rays
- 2D projections \rightarrow reconstruct in 3D
- Complete axial coverage and ~14 cm longitudinal coverage

Double orbit imaging proposal

Objective: extend the longitudinal coverage of our CBCT images by implementing a protocol involving multiple scans in series

Double orbit procedure



- Step and shoot modality
 - Standard protocol: scan superior to inferior
- Abut region: 1.5 cm wide
 - Essential for 3D to 3D image registration
 - Corrects for patient movement

Previous double orbit results





Head and neck patient; single orbit (~14 cm)

Head and neck patient; double orbit (~27 cm)

How does this new imaging technique affect the patient?

- Additional absorbed radiation dose
 - We want to obtain a geometric profile of the dose distribution at the center and at the periphery
- CTDI: computed tomography dose index
 - Acrylic material is analogous to the human body
- Thermoluminescent dosimeters



Thermoluminescent dosimeters (TLD)

Irradiation



Measurement



Conduction band (unstable)

Electron trap Valence band (stable)



- LiF TLD chips
 - 1/8 inch square by 30/1000 inch depth
- Each chip measures the absorbed radiation for a single point
 - Radiation causes chemical reaction
 - Latent measurement tool

Preliminary tests

- Limitations
 - Their response is energy dependent
 - Non-uniformity of individual chips
- Certain characteristics of our TLD batch were assessed before acquiring data
 - Uniformity of response
 - Linearity of response to dose
 - Reproducibility does each TLD respond to radiation consistently?

TLD processing steps



read and recorded individually

Preliminary assessments

- The standard deviation (uniformity) of the TL readings decreased with increased dose
 - Due to the deposition of more photons
 - More photons = higher TL readout
- Our batch showed sufficient linearity in response and reproducibility



Relating the TL reading to absolute absorbed dose

Harshaw 3500 TLD reader



- The absolute dosimetry of TLDs is not apparent
- Readout in nano-Coulombs
- Convert the nC to absolute dose unit

Ion chamber (IC) calibration

- Place ion chamber inside a disk shaped water phantom (analogous to CTDI acrylic);
 5 TLDs set adjacent to the IC
- Perform one double CBCT scan
- Connect ion chamber to electrometer (outputs a reading)





Absolute dose calculation

AAPM (American Association of Physicists in Medicine) protocol for absolute dose calculation from in-water ion chamber readings (M)

$$D_w = MN_k P_{qcham} P_{sheath}$$

Dose to water is calculated in Gy
 D_w = 10.29 cGy for one double CBCT

TLD calibration

- Avg TL readout: 51.94 nC
- Calibration factor:
 - 51.94 nC \approx 10.29 cGy absolute dose

Head and neck patient simulation



Sensitive area is increased by placing the two phantoms in series; allows for complete coverage of a double CBCT

Custom modifications

ThreeCustom holders designed to harbor TLDs

- 33cm (CAX)
- 15 cm
- 16 cm



Setup

- After annealing, two TLDs were placed in each well of the holders
- Holder placement:
 - Long 33 cm holder: central axis
 - 16 cm holder: peripheral channel head phantom
 - 15 cm holder: peripheral channel body phantom

Double Cone beam CT acquisition

- Beam isocenter (first scan): 12 cm from the sup. axial surface
 - Beam length: 13.8 cm (6.9 cm on either side of the isocenter)
 - Isocenter placement accounts for beam scatter
- Second CBCT scan: shift the patient
 - Clinical procedure: 12.3 cm shift
- 4 double cone beam CT scans were performed
 - 8 scans total



Conclusions

- The overlap in the abut region causes a marked increase in the absorbed dose
 - Is the extra dose warranted?
- Next step: Investigate methods of lowering the resulting absorbed dose while maintaining the integrity of our images
 - Develop better image registration techniques
 - Experiment with lowering the current-time (mA's) product through the x-ray tube

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